

# ANALYSING EEG SIGNAL TO RECOGNISE EMOTIONS

Dissertation Phase 2 Report

*Submitted by*

Mr. DILISH JOSE

REG NO : TKM22MEAI07

*In partial fulfillment for the award of the degree of*

MASTER OF TECHNOLOGY

IN

Artificial Intelligence

Under the guidance of

Dr. Mubarak Ali M



Centre for Artificial Intelligence

TKM College of Engineering, Kollam

JUNE 2024

Thangal Kunju Musaliar College of Engineering  
Centre for Artificial Intelligence



C E R T I F I C A T E

This is to certify that, this report titled ***ANALYSING EEG SIGNAL TO RECOGNISE EMOTIONS*** is a bonafide record of the **Dissertation Phase-2** work presented by **DILISH JOSE (TKM22MEAI07)**, under our guidance and supervision, in partial fulfillment of the requirements for the award of the degree, **M. Tech in Artificial Intelligence** in **APJ Abdul Kalam Technological University**.

Internal Supervisor

Co-Supervisor and Project Coordinator

Dr. Mubarak Ali M  
Assistant Professor  
Department of ME  
TKMCE

Dr. Sumod Sundar  
Associate Professor  
Centre for AI  
TKMCE

Head of the Department

Dr. Imthias Ahamed T P  
Professor  
Centre for AI  
TKMCE

## ACKNOWLEDGEMENT

A successful project is a fruitful culmination of efforts by many people, some directly involved and some others indirectly, by providing support and encouragement. Firstly I would like to thank the almighty for giving me the wisdom and grace for making my project a memorable one. I thank him for steering me to the shore of fulfillment under his protective wings.

I express my sincere gratitude to **Dr. T A Shahul Hameed**, Principal of T.K.M College of Engineering for allowing me to present my Dissertation Phase 2. I would like to thank **Dr. Imthias Ahamed T P**, Professor and Head of the Department, Centre for Artificial Intelligence, TKM College of Engineering, Kollam, for his constant support and encouragement throughout the work.

With a profound sense of gratitude, I would like to express my heartfelt thanks to my Internal Supervisor **Dr. Mubarak Ali M**, Assistant Professor, Department of Mechanical Engineering, TKM College of Engineering, Kollam, Co-Supervisor and Project Co-ordinator, **Dr. Sumod Sundar**, Associate Professor, Centre for Artificial Intelligence(AI), TKM College of Engineering, Kollam , **Dr. Muhammed Shanir P P**, Associate Professor, Department of EEE, TKM College of Engineering, Kollam for his expert guidance, cooperation, and immense encouragement. I also extend my thanks to the entire faculty and staff members of the Centre for AI, TKMCE, who have encouraged me throughout this work.

I also express my thanks to my loving parents and friends, for their support and encouragement in the successful completion of this work.

Dilish Jose

## Abstract

Emotion recognition through Electroencephalography (EEG) is widely acknowledged as a reliable method with diverse applications including defense, aerospace, and medical domains. This research aims to detect emotions from EEG signals, depicting individuals' brain activity. Electroencephalogram (EEG) serves as a pivotal tool in Brain-Computer Interface (BCI) systems, capturing brain signals. With the advancement of machine learning algorithms and the growing real-world utility of BCIs, the classification of emotions from EEG data has gained prominence. Previously, researchers had limited insights and knowledge into the specific connections between distinct EEG characteristics and various emotional states. This work utilizes the DEAP dataset, featuring 32 EEG recording channels, and employs ensemble models for training. The model's performance is evaluated using metrics like accuracy, precision, recall, and F1-score. In this work, we augment traditional feature extraction methods such as mean, standard deviation, entropy, skewness, and kurtosis along with continuous wavelet transformation for enhanced signal analysis. This combined approach aims to capture both basic characteristics and time-frequency domain information within the EEG signals, potentially improving emotion classification accuracy.

# Contents

<b>1</b>	<b>Introduction</b>	<b>1</b>
<b>2</b>	<b>Literature Survey</b>	<b>5</b>
<b>3</b>	<b>Methodology</b>	<b>13</b>
3.1	Objectives . . . . .	13
3.2	Proposed Framework . . . . .	13
3.3	Dataset used . . . . .	14
3.3.1	DEAP DATASET . . . . .	14
3.4	Techniques Used . . . . .	15
3.4.1	Data Preprocessing . . . . .	15
3.4.2	Feature Extraction . . . . .	18
3.4.3	Continuous Wavelet Transform (CWT) . . . . .	20
3.5	Convolutional Neural Networks . . . . .	23
3.6	Performance Metrics . . . . .	25
<b>4</b>	<b>Experimental Analysis and Results</b>	<b>27</b>
4.1	Experiments on data pre-processing task . . . . .	27
4.2	Environmental Setup . . . . .	28
4.3	Signal Analysis . . . . .	28
<b>5</b>	<b>Conclusion and Future Scope</b>	<b>39</b>
	<b>References</b>	<b>42</b>

# List of Figures

1.1	Valence - Arousal Model . . . . .	2
3.1	Proposed Framework . . . . .	13
3.2	Scalogram images from 4 quarters of valence-arousal model for DEAP database	23
4.1	Accuracy vs Epoch on 1st approach . . . . .	29
4.2	Loss vs Epoch on 1st approach . . . . .	30
4.3	Accuracy/Loss vs Epoch on 1st approach . . . . .	31
4.4	Accuracy vs Epoch on 2nd approach . . . . .	32
4.5	Loss vs Epoch on 2nd approach . . . . .	33
4.6	Accuracy/Loss vs Epoch on 2nd approach . . . . .	34
4.7	Confusion matrix of second approach . . . . .	36

# List of Tables

3.1	Class Labels . . . . .	15
3.2	Model Architecture . . . . .	24
4.1	Classification report of 1st approach . . . . .	32
4.2	Classification report of the second approach . . . . .	35
4.3	Comparison between existing works . . . . .	37

# Chapter 1

## Introduction

Emotion is a complex and multifaceted psychological and physiological phenomenon that encompasses a range of subjective experiences, feelings, and behavioral responses. It is a fundamental aspect of human nature, influencing various aspects of cognition, decision-making, and interpersonal interactions. Emotions typically involve a combination of physiological changes, such as alterations in heart rate, facial expressions, and hormonal levels, along with subjective experiences like joy, sadness, fear, anger, and surprise. With the advancement of Artificial Intelligence and Deep Learning techniques, emotion recognition has wide applications with respect to the field of human-computer interaction. Many researchers are now more interested as a result of this. feeling recognition using text, speech, posture, and facial expression is becoming more and more popular; nonetheless, these techniques are all individualistic and cannot guarantee the authenticity of feeling. Research in psychology and physiology has demonstrated that physiological signals—rather than voice, posture, or facial expressions—are a better indicator of an individual’s genuine emotional state. Nonetheless, recorded physiological signals like EOG, ECG, and EMG continue to be indirect reactions brought on by emotions. Low accuracy in detecting emotions is caused by inappropriate evaluation criteria.

Electroencephalogram (EEG) signals are recordings of the brain’s spontaneous electrical activity, typically obtained by placing electrodes on the scalp. These signals depict the neural oscillations and patterns of electrical activity resulting from neuron firing in the brain. Studies in neurophysiology and psychology suggest that EEGs not only reflect various forms of brain activity and the brain’s functional state but also provide valuable insights into a person’s emotional state. Emotion development or activity is closely associated with cerebral cortex activity, making EEG signals a valuable tool for emotion recognition. In recent years, EEG signals have increasingly been integrated into emotion recognition research due to their objectivity and high accuracy in classification.

In the evolving realms of neuroscience and machine learning, there is a growing emphasis on the endeavor to decode and analyze human emotions through Electroencephalogram (EEG) data, marking a pivotal research objective. EEG is at the forefront of brain-computer interface (BCI) technologies because it is a non-invasive tool for capturing the complexities of brain activity. The convergence of machine learning developments with the growing use of BCIs in real-world contexts has sparked intense interest in the exact categorization of

emotions using EEG data. Here we use DEAP dataset. The DEAP dataset comprises 1280 data instances collected from 32 individuals, each consisting of 40 trials. The primary focus lies on evaluating emotions based on Valence and Arousal dimensions, which serve as fundamental criteria. These dimensions form a two-dimensional plane, organizing emotional states into four quadrants based on varying levels of Valence and Arousal as mentioned in Fig. 1.1. Each quadrant corresponds to a distinct emotion classification, establishing a structured framework for categorizing emotional states by considering the intricate relationship between Valence and Arousal levels.

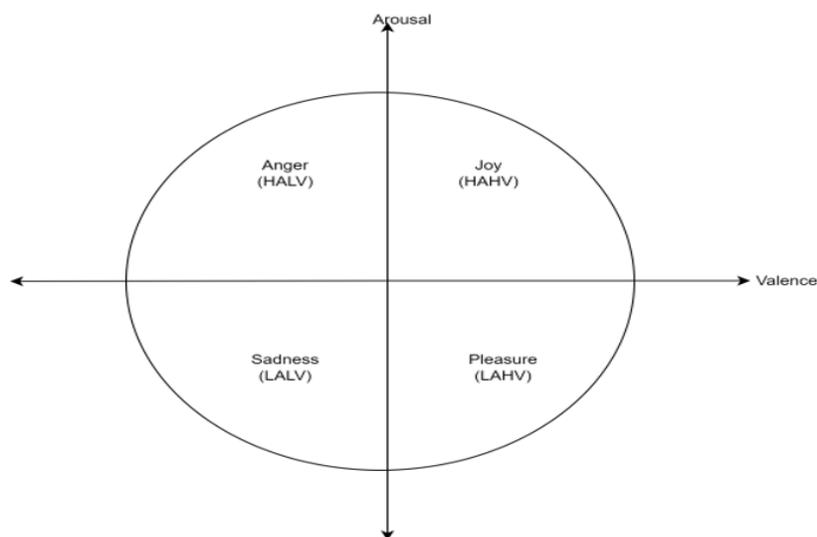


Figure 1.1: Valence - Arousal Model

While traditional feature extraction techniques provide valuable insights, they often fail to capture the crucial time-frequency information embedded within EEG signals. Continuous wavelet transformation (CWT) addresses this limitation by decomposing the signal into time-frequency components, enabling the analysis of how specific frequencies evolve over time. By incorporating CWT features alongside standard features such as mean, standard deviation, entropy, skewness, and kurtosis, a more comprehensive picture of the emotional state reflected in the EEG data can be obtained. This combined approach aims to enhance the accuracy and robustness of emotion classification models, ensuring a deeper and more precise understanding of emotional states.

The use of ensemble models as the training method represents a deliberate and strategic synthesis of various algorithms, with the primary goal of leveraging their combined strengths to achieve enhanced predictive performance. Ensemble methods, which integrate multiple learning algorithms, are specifically designed to improve the robustness and accuracy of predictive models. This strategy effectively mitigates the limitations associated with relying on a single algorithm. In the context of emotion recognition based on EEG data, the complex patterns and intricacies of the data can be better captured through the collaborative effort of different models.

By employing ensemble models, the research harnesses the diversity of multiple algorithms to create a more resilient and reliable predictive system. Each algorithm within the ensemble contributes its unique perspective on the data, leading to a more nuanced and accurate classification of emotional states. This approach is particularly beneficial in handling the variability and complexity inherent in EEG signals, which reflect the dynamic and multifaceted nature of human emotions.

Integrating CWT features with traditional statistical features further enhances the model's ability to detect subtle patterns in EEG data. The CWT allows for a detailed examination of the signal's temporal and frequency characteristics, providing insights that might be missed by conventional feature extraction techniques. This comprehensive analysis contributes to a more robust understanding of the emotional states being studied, leading to improved model performance.

The constructed ensemble model for emotion recognition using EEG data will undergo thorough evaluation using key metrics: accuracy, precision, recall, and F1-score. Accuracy will measure the overall correctness of the model's emotion class predictions. Precision will measure the proportion of true positive predictions among all positive predictions, reflecting the model's ability to reduce false positives. Recall will gauge the proportion of actual positive cases correctly identified by the model, indicating its effectiveness in capturing true positives. The F1-score, the harmonic mean of precision and recall, will offer a balanced evaluation of the model's performance, particularly useful for managing imbalanced datasets.

These evaluation metrics will serve as benchmarks, offering a complete assessment of the model's capacity to reliably recognize and categorize emotions based on EEG data. By thoroughly analyzing these metrics, researchers can evaluate how effectively the ensemble approach manages the complexities of EEG signals, thereby enabling reliable and precise emotion recognition. This systematic assessment will provide valuable insights into the model's strengths and areas for potential improvement, guiding iterative refinements to achieve optimal predictive performance.

The integration of ensemble models for emotion recognition using EEG data represents a sophisticated and strategic approach, leveraging the combined strengths of multiple algorithms to enhance predictive performance. This method is particularly suited to the complexities of EEG signals, which provide a detailed representation of brain activity related to emotions. The DEAP dataset, focusing on Valence and Arousal dimensions, serves as a foundational framework for this analysis. By incorporating Continuous Wavelet Transformation (CWT) features alongside traditional statistical features, the approach aims to capture a comprehensive picture of emotional states.

Rigorous evaluation of the model using metrics like accuracy, precision, recall, and F1-score will benchmark its effectiveness, offering valuable insights into its performance and informing further refinements. This systematic approach aims to advance emotion recognition by providing robust and accurate emotion classification based on EEG data. The DEAP dataset, with its focus on Valence and Arousal dimensions, ensures the analysis is grounded

in a well-established framework, thereby enhancing the reliability of the findings.

Moreover, this advanced methodological framework for emotion recognition using EEG data signifies a significant step forward in the field. By meticulously assessing the model's performance through a comprehensive set of metrics, researchers can develop a deeper understanding of the model's capabilities and limitations. This process will not only improve the current model but also set a precedent for future research, emphasizing the importance of robust evaluation and continuous refinement in the development of emotion recognition technologies based on EEG data.

In summary, the continuous innovation and exploration in EEG signal processing and emotion recognition methodologies hold great potential for advancing the field and opening up new avenues for practical applications. These advancements could revolutionize areas such as mental health care by enabling personalized and real-time emotional monitoring and interventions, enhancing human-computer interaction by creating more responsive and adaptive systems, and contributing to other domains like education, marketing, and entertainment. As researchers continue to push the boundaries of technology and methodology, the future of emotion recognition from EEG signals looks promising, with the potential to significantly impact and improve various aspects of human life and interaction.

## Chapter 2

# Literature Survey

Several studies have contributed significantly to the development of emotion recognition through EEG signals. These studies have employed various techniques and datasets to achieve high levels of accuracy.

The work conducted by Zhang, Zhang, and Ji [1] introduced a novel approach to emotion classification utilizing EEG data. This innovative method leverages Empirical Mode Decomposition (EMD) and Autoregressive (AR) modeling, achieving an impressive average recognition rate of 86.28% across four binary-class tasks using the DEAP dataset. By focusing on feature extraction through EMD and AR modeling, this method demonstrated competitive performance in emotion recognition compared to existing techniques, suggesting its significant potential for practical applications in real-world scenarios where accurate emotion detection is essential.

The methodology employed in this work involves decomposing EEG signals into Intrinsic Mode Functions (IMFs) using EMD. This step is crucial as it allows the analysis of the complex, non-linear, and non-stationary properties inherent in EEG data, which traditional linear methods often fail to address effectively. Once the EEG signals are decomposed into IMFs, the AR model is applied to each IMF using a sliding window approach. This approach captures the dynamic temporal features of the EEG signals, providing a comprehensive feature set for emotion classification.

These features, represented by the AR coefficients, are then input into a Support Vector Machine (SVM) classifier for the final emotion recognition task. The choice of SVM is strategic due to its effectiveness in handling high-dimensional feature spaces and its robustness in binary classification tasks. The work's use of the DEAP dataset, which contains EEG and peripheral physiological signals from 32 participants, underscores the empirical validation of the proposed method and its potential for broader application.

The DEAP dataset provides a rich and diverse set of data, including both EEG and peripheral physiological signals, which enhances the robustness of the model's training and validation processes. This comprehensive dataset enables the researchers to thoroughly evaluate the performance of their proposed method across different emotional states and participants, ensuring that the results are both reliable and generalizable.

Overall, the work's findings indicate that the proposed EMD and AR model-based method offers a promising approach to emotion recognition using EEG signals. Its competitive performance compared to existing techniques highlights its potential for practical applications, such as in affective computing, mental health monitoring, and human-computer interaction. Future research could further explore the integration of this method into a pleasure-arousal-dominance framework and investigate the impact of additional features, potentially enhancing the model's accuracy and applicability in various real-world scenarios.

Li, Huang, Zhou, and Zhong [2] proposed a unique method for emotion recognition utilizing EEG signals, introducing a hybrid deep neural network termed Convolutional and LSTM Recurrent Neural Networks (CLRNN). This innovative approach integrates spatial characteristics, frequency domain, and temporal features into EEG Multidimensional Feature Images (EEG MFI), enabling a comprehensive representation of the emotional variations captured in EEG data. The authors report a significant improvement in emotion classification accuracy, achieving an average of 75.21% on the DEAP dataset, a well-known benchmark for evaluating emotion recognition systems.

The CLRNN architecture combines Convolutional Neural Networks (CNN) and Long Short-Term Memory (LSTM) Recurrent Neural Networks (RNN), controlling the strengths of both network types. The CNN component is adept at extracting spatial features from the EEG MFI sequences, capturing the spatial distribution of EEG signals across different channels. This is followed by a max pooling stage to aggregate information and reduce dimensionality. The resultant features are then flattened into a one-dimensional vector and fed into the LSTM unit, which excels at modeling temporal dependencies, crucial for understanding the dynamic nature of emotional states over time. This dual approach allows the CLRNN to effectively process the complex, multi-dimensional data inherent in EEG signals.

The CNN employed in this model utilizes 30 filters in its initial layer to extract a diverse set of features, incorporating multiple receptive field sizes to capture various spatial characteristics. This meticulous design allows the CNN to handle the spatial distribution of EEG signals efficiently. Following the CNN layers, the LSTM RNN models the context information from the long-term EEG MFI sequences, crucial for understanding the temporal evolution of emotional states. The LSTM outputs the emotion states through a softmax activation function, completing the classification process.

The CLRNN model offers a significant advantage by seamlessly integrating spatial, frequency, and temporal characteristics of EEG signals. This comprehensive approach leads to notable enhancements in emotion classification accuracy compared to existing state-of-the-art methods. The hybrid architecture adeptly captures the intricate patterns within EEG signals, which are pivotal for precise emotion recognition. The study underscores the robust performance of the CLRNN model, achieving an average emotion classification accuracy of 75.21%. This surpasses the performance of other methods such as CNN RNN (69.58%), Support Vector Machine (SVM) (67.45%), Random Decision Forest (45.47%), and k-Nearest Neighbors (k-NN) (62.84%). Particularly noteworthy is Subject 4's achievement of the highest accuracy at 90.54% with the CLRNN model, highlighting its potential for achieving high

accuracy in individual cases.

Despite the detailed discussion on the advantages, the work does not extensively discuss potential challenges associated with the implementation of the CLRNN model. There is a notable absence of commentary on the practical difficulties that may arise during deployment, such as computational resource demands, real-time processing capabilities, and the need for extensive training data to achieve optimal performance. Furthermore, the work does not address potential generalization issues that might occur when applying the model to different datasets or real-world scenarios, where external factors like environmental noise, individual differences in EEG signal patterns, and the variability of emotional expressions can significantly impact classification accuracy.

Despite these limitations, the authors highlight the potential applications of their method in fields such as mental health care and entertainment. The ability to monitor and recognize emotional states accurately could lead to advancements in personalized mental health interventions and enhance user experiences in interactive entertainment systems. The real-world applicability of the CLRNN model emphasizes its importance, although future research should aim to address the identified gaps, focusing on overcoming implementation challenges and ensuring robust generalization across diverse conditions.

Islam et al.[3] presented a comprehensive review of EEG-based emotion recognition systems, examining both deep learning and shallow machine learning techniques. Their work evaluates and compares various methods, classifiers, the number of emotions classified, accuracy rates, and datasets employed, aiming to provide insights for future research in this field. The work summarizes common steps and methodologies used in state-of-the-art emotion recognition systems, offering a detailed comparison between deep learning-based and shallow machine learning-based approaches. It highlights important issues and recommendations regarding classifiers, feature extraction, and datasets.

The architecture of the model for emotion recognition from EEG signals encompasses a comprehensive workflow involving data management, preprocessing, feature extraction, feature selection, and the utilization of classification algorithms. This multifaceted approach is crucial for accurately discerning the subtle signals that indicate human emotions. In recent times, deep learning techniques such as Convolutional Neural Networks (CNN), Deep Belief Networks (DBN), and Recurrent Neural Networks (RNN) have demonstrated significantly greater efficacy for extracting emotions from EEG data compared to shallow learning algorithms like k-Nearest Neighbors (kNN), Naive Bayes (NB), and Random Forest (RF). The superior performance of deep learning models is evident from their higher accuracy rates in tasks related to emotion recognition.

Despite these advancements, there are notable disadvantages and gaps in the current literature. Many studies do not explicitly detail the feature extraction methods or classification algorithms they employ, posing challenges for reproducibility and validation of results. Additionally, while deep learning models have demonstrated promising results, their high computational resource demands and the necessity for large datasets for training can be limiting factors.

Results from various studies consistently show that deep learning techniques, especially CNN-based systems, outperform shallow learning-based systems in emotion recognition from EEG signals. The average accuracy of deep learning models has remained superior over six consecutive years, from 2015 to 2020. However, the identifies several areas for future work to further enhance emotion recognition systems. These include addressing classifier-related issues, improving feature extraction techniques, and refining the datasets used. Specifically, it suggests focusing on the subtraction of baseline EEG data from emotionally aroused EEG data to achieve more accurate results.

The data used in the reviewed work predominantly come from publicly available datasets such as DEAP, SEED, and MAHNOB. The DEAP dataset is particularly noted for its extensive use in emotion recognition research. Some researchers have also generated their own datasets to advance their studies. However, the work highlights certain limitations, such as the failure of some researchers to subtract baseline EEG data from emotionally aroused data, potentially affecting the accuracy of their results. Additionally, the lack of explicit mention of feature extraction methods or classification algorithms in some articles hinders the reproducibility of their findings.

In conclusion, Islam et al.'s review provides valuable insights into the performance of deep learning and shallow machine learning-based emotion recognition systems, emphasizing the differences in accuracy depending on the datasets used. For future research, the work recommends focusing on overcoming classifier-related challenges, improving feature extraction techniques, and refining datasets to enhance the accuracy and reliability of emotion recognition systems. By addressing these areas, the field can advance towards more robust and practical applications of emotion recognition from EEG signals. The practical implications of this review include guidance for beginners in developing effective emotion recognition systems and recommendations for future research directions, highlighting the effectiveness of deep learning techniques like CNN, DBN, and RNN compared to shallow learning-based algorithms. The review underscores the significance of emotion recognition from EEG signals for Human-Computer Interaction systems, emphasizing the utilization of sophisticated techniques like deep learning to overcome challenges associated with the small amplitude of EEG signals.

Chen et al. [4] have made a substantial contribution to the field of EEG-based emotion recognition by seamlessly integrating Deep Convolutional Neural Networks (CNN) with shallow machine learning models. Their approach focuses on automating the extraction of intricate feature representations from raw EEG data to improve the accuracy of emotion classification. Through meticulous experimentation and analysis, the work meticulously explores various aspects of their methodology, including fine-tuning specific parameters in deep CNN models, implementing data preprocessing techniques, EEG feature extraction methods, utilization of shallow machine learning classifiers, and the application of deconvolutional networks to visualize hidden features.

Central to their methodology is the utilization of the DEAP dataset, a comprehensive repository of EEG data from 32 subjects, for conducting extensive testing and validation

experiments. They use deep convolutional neural networks to classify binary emotions by using features that are taken from the frequency and time domains, as well as from their combinations. Additionally, they use deconvolutional networks, deep CNN models, and shallow machine learning classifiers for a range of EEG-based emotion categorization applications. The work rigorously employs a 10-fold cross-validation approach for each type of feature collected from each individual to ensure the robustness and reproducibility of their findings.

The work's foundation lies in the utilization of the DEAP dataset, enabling comprehensive preprocessing steps to extract features from different domains and ensure a balanced representation for classification purposes. The construction of the test set involves meticulous random extraction of high-class and low-class labels, with the remaining data partitioned for training and verification. Each type of feature extracted from each subject undergoes 10-fold cross-validation, ensuring thorough training and testing of the models. This meticulous approach ensures the validity and generalizability of their findings.

The results of the work are presented through comprehensive testing experiments and subsequent analysis, including meticulous comparisons with state-of-the-art shallow classifiers. Additionally, the work also uses deconvolution procedures to view the reconstructed EEG patterns that underlie the hidden units that are most active, which offers important insights into the inner workings of the model. Such insights deepen our understanding of how deep learning models interpret EEG data and contribute to the advancement of the field.

In conclusion, Chen et al.'s research demonstrates the effectiveness of utilizing deep CNN models for EEG-based emotion recognition tasks. By seamlessly integrating deep learning techniques with traditional shallow classifiers, the work achieves significant advancements in emotion classification accuracy. The comprehensive evaluation and analysis presented in their work offer invaluable guidance for both researchers and practitioners seeking to leverage similar techniques for emotion recognition applications in real-world scenarios.

In 2020, Garg and Verma [5] proposed a novel wavelet-based Deep Learning framework aimed at enhancing EEG-based emotion recognition by capturing both frequency and spatial characteristics of multichannel EEG signals. Their work introduced Scalogram features and utilized the GoogleNet model for emotion classification in two/three-dimensional space, particularly emphasizing the analysis of affective states in Valence and Arousal dimensions. By leveraging the DEAP dataset and employing Continuous Wavelet Transform with the 'Generalized Morse Wavelet family' for feature extraction, the proposed framework demonstrated promising results, particularly excelling in Valence classification. The work highlighted the importance of considering both frequency and spatial characteristics of EEG signals, demonstrating the effectiveness of the GoogleNet model in identifying affective states from Scalogram representations of EEG data.

The contributions of Garg and Verma's work include the development of a wavelet-based Deep Learning framework tailored for emotion recognition, incorporating Scalogram features and the GoogleNet model for classification in two/three-dimensional space. By analyzing affective states using multimodal data and focusing on Valence and Arousal dimensions, their approach offers practical implications in various fields such as healthcare, human-computer

interaction, and affective computing.

The introduction of their work emphasizes the significance of integrating frequency and spatial characteristics of EEG signals to improve emotion recognition. They employ a methodology that preprocesses multimodal EEG signals using wavelet analysis and then utilizes deep learning techniques for classification. To extract features, they utilize Continuous Wavelet Transform with the 'Generalized Morse Wavelet family' and employ Scalogram features in conjunction with the GoogleNet model for emotion recognition across two or three dimensions.

Garg and Verma's study employed the DEAP dataset, which includes multichannel EEG signals and peripheral physiological signals from 32 subjects, with feedback recorded on a continuous 9-point scale for valence, arousal, dominance, and liking. Their results demonstrated high accuracy rates, especially in valence classification, achieving 92.19% accuracy for distinguishing between two classes (High Valence and Low Valence).

In conclusion, Garg and Verma's work provides valuable insights into EEG-based emotion recognition, emphasizing the importance of considering both frequency and spatial characteristics of EEG signals. While showcasing promising results, their work acknowledges limitations such as the focus on valence-arousal space and reliance on the DEAP database. Future research directions suggested include exploring other dimensions of emotions and evaluating the proposed model's performance with diverse datasets and classification techniques.

Topic and Russo [6] have made a notable contribution to the field of EEG-based emotion recognition by developing innovative methodologies that significantly advance the domain. A key insight from their research is the importance of simultaneously considering both the frequency and spatial characteristics inherent in EEG signals. By integrating wavelet-based feature extraction techniques, deep learning architectures, and sophisticated classification algorithms, Topic and Russo effectively extract nuanced information from EEG data. This approach results in more accurate and reliable emotion classification, demonstrating the power of combining these advanced techniques.

The work by Topic and Russo also emphasizes the potential for real-world applications of EEG-based emotion recognition systems. By showcasing high accuracy rates and robust performance in classifying affective states, their research opens the door for practical implementations across various domains. For instance, in the field of mental health care, such systems could revolutionize the monitoring and management of emotional states, leading to personalized interventions and improved patient outcomes. Similarly, in the realm of human-computer interaction, these systems hold promise for enhancing user experiences by enabling more intuitive and responsive interfaces that adapt to users' emotional states in real-time.

Despite the substantial progress achieved by Topic and Russo, they also highlight the need for further research to explore diverse datasets and classification techniques. While their proposed methodologies have shown promising results, the generalizability of these methods across different datasets and contexts remains a topic of ongoing investigation.

The authors acknowledge the importance of exploring alternative classification techniques and refining existing methodologies to enhance the robustness and reliability of EEG-based emotion recognition systems.

In summary, the findings from Topic and Russo pave the way for enhanced applications in fields ranging from mental health care to human-computer interaction. By advancing the understanding of EEG-based emotion recognition and introducing innovative methodologies, the authors are poised to unlock new possibilities for leveraging EEG signals to promote human well-being and technological advancement. Their research highlights the potential for EEG-based systems to make significant contributions to various practical applications, demonstrating the versatility and impact of their innovative approaches.

Collectively, Topic and Russo's work represents significant advancements in the field of EEG-based emotion recognition. Their work underscores the importance of considering both frequency and spatial characteristics of EEG signals, showcases the potential for real-world applications, and underscores the necessity for further research to ensure broad applicability and improved performance. By integrating deep learning with traditional classification techniques, the authors have set a new standard in the domain, providing a robust foundation for future research and practical implementations.

In 2018 Mert and Akan [7] make significant strides in the domain of EEG-based emotion recognition through their innovative use of Multivariate Empirical Mode Decomposition (MEMD). Their work offers a comprehensive approach to decomposing EEG signals, which are inherently nonstationary, into Intrinsic Mode Functions (IMFs). This method enables detailed analysis and extraction of valuable features for emotion recognition.

Their methodology involves several advanced signal processing techniques. By applying MEMD, they decompose EEG signals into IMFs, which are then analyzed using power ratio, power spectral density (PSD), entropy, Hjorth parameters, and correlation. To manage the high dimensionality of the resulting feature set, they employ Independent Component Analysis (ICA), reducing it to a more manageable size. This refined feature set is then used to train k-nearest neighbor (k-NN) and artificial neural network (ANN) classifiers, evaluated through a Leave-One-Out (LOO) cross-validation scheme.

Mert and Akan's approach is rigorously tested on the DEAP dataset, a widely used benchmark in affective computing. This dataset includes EEG recordings from participants watching music videos, with self-assessed valence and arousal scores providing ground truth for emotional states. The authors' MEMD-based method demonstrates superior performance compared to previous studies, achieving higher accuracy rates for both arousal and valence classification. Specifically, the k-NN classifier yields 51.01% accuracy for arousal and 67% for valence, while the ANN classifier achieves 75% and 72.87% for arousal and valence, respectively. Notably, the method achieves the highest arousal accuracy of 95% for one participant, illustrating its potential for precise emotion recognition.

The work underscores the effectiveness of MEMD in handling the complex nature of EEG signals. By decomposing these signals into IMFs, Mert and Akan can capture both temporal

and spectral features essential for distinguishing emotional states. Their use of ICA further refines the feature extraction process, enhancing the classifiers' ability to accurately recognize emotions. The results indicate that MEMD, combined with robust feature extraction and classification techniques, offers a powerful tool for EEG-based emotion recognition.

In conclusion, Mert and Akan's research contributes valuable insights and methodologies to the field of affective computing. Their MEMD-based approach not only advances the understanding of how to process and analyze EEG signals for emotion recognition but also sets a benchmark for future studies. Their findings highlight the potential for applying such techniques in real-world applications, ranging from mental health monitoring to enhancing human-computer interaction. This work represents a significant step forward in leveraging the intricate details of EEG signals to decode human emotions accurately.

These studies collectively represent significant strides in the field of EEG-based emotion recognition, introducing novel methodologies that have propelled the domain forward. A pivotal insight garnered from these studies is the critical consideration of both the frequency and spatial characteristics inherent in EEG signals. Through the integration of wavelet-based feature extraction techniques, deep learning architectures, and sophisticated classification algorithms, researchers have showcased their ability to extract nuanced information from EEG data, thereby enabling more precise and dependable emotion classification.

Furthermore, these studies underscore the potential for real-world applications of EEG-based emotion recognition systems. By demonstrating high accuracy rates and robust performance in classifying affective states, researchers have paved the way for practical implementations across various domains. For instance, the deployment of these systems in mental health care holds the promise of revolutionizing the monitoring and management of emotional states, leading to personalized interventions and improved patient outcomes. Similarly, in the realm of human-computer interaction, these systems offer the potential to enhance user experiences by enabling more intuitive and responsive interfaces capable of adapting to users' emotional states in real time.

However, despite the substantial progress achieved, these studies also emphasize the necessity for further research to explore diverse datasets and classification techniques. While the methodologies proposed in these studies have demonstrated promising results, their generalizability across different datasets and contexts remains an ongoing area of investigation. Additionally, researchers acknowledge the importance of exploring alternative classification techniques and refining existing methodologies to enhance the robustness and reliability of EEG-based emotion recognition systems.

In summary, the findings from these studies lay the groundwork for enhanced applications in fields ranging from mental health care to human-computer interaction. By advancing our understanding of EEG-based emotion recognition and introducing innovative methodologies, researchers are poised to unlock new possibilities for leveraging EEG signals to promote human well-being and technological advancement.

# Chapter 3

## Methodology

### 3.1 Objectives

- To analyse the dataset using different data analytic techniques.
- To design a deep learning model to classify emotions.

### 3.2 Proposed Framework

Figure 3.2 shows the proposed framework used in the work.

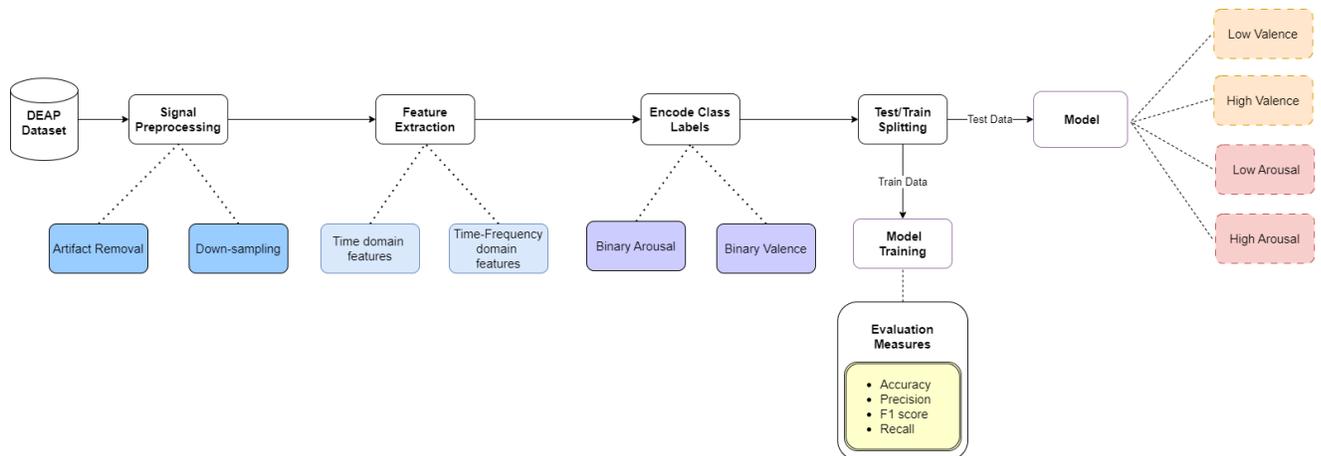


Figure 3.1: Proposed Framework

Utilizing the DEAP Dataset, the process begins with comprehensive signal processing to enhance data quality. This includes preprocessing steps such as frequency downsampling and artifact removal to ensure the integrity of the data. Subsequently, a thorough data analysis is conducted to identify patterns and trends within the preprocessed signals. Feature extraction techniques are then applied to isolate relevant information from the signals, focusing on both time domain and frequency domain features. Following feature extraction, feature

selection methods are employed to optimize model performance by selecting the most discriminative features. The model undergoes rigorous training using the selected features, and during testing, it proficiently classifies data into four classes: high arousal, high valence, low arousal, and low valence. Evaluation measures are employed throughout both the training and testing phases to assess the model's accuracy and effectiveness, ensuring robust performance in emotion classification tasks.

### 3.3 Dataset used

The following dataset is used for the experimentation.

- DEAP (Dataset for Emotion Analysis using Physiological Signals) Dataset

#### 3.3.1 DEAP DATASET

The DEAP dataset is used for the experiment. A group of researchers from Queen Mary University of London created the DEAP dataset. It is a sizable, publicly available dataset that includes both emotional assessments and a variety of physiological signs. Research in affective computing, emotion recognition, and related domains frequently makes use of the DEAP dataset. It offers a useful tool for creating and assessing models and algorithms for classifying emotions and comprehending the physiological underpinnings of emotional states. The researchers used 32 people to watch 40 trials of music videos while they monitored and recorded induced EEG, ECG, EMG, and other bioelectrical signals for their data gathering experiment. Every video, featuring varying emotional inclinations, was watched for around 60 seconds. The participants then assessed the movies for arousal, valence, liking, and dominance on a scale from 1 to 9. Ratings for each dimension represent different facets of emotion and range from 1 (low) to 9 (high). While valence assesses how pleasant the stimulus is, ranging from unpleasant or depressing to joyful or jubilant, arousal describes the degree of feeling evoked by the stimuli, ranging from bored to excited.

The EEG signals from the DEAP dataset were downsampled to 128 Hz, filtered from 4.0 Hz to 45 Hz, and eye artifacts were removed using the blind source separation approach. For each trial, a 63-second signal is captured, with the first 3 seconds representing pre-trial baseline deleted data, and the remaining 60 seconds representing trial data. The DEAP dataset consists of 1280 data samples for 32 individuals, each containing 40 trials. Major focus is on Valence and Arousal as criteria for emotional evaluation, using these two dimensions to establish emotional labels.

The class labels presented in the table 3.1, is derived from the EEG dataset's valence and arousal columns. Following video trials, valence and arousal values (ranging from 1 to 9) are assigned for emotion recognition. Utilizing these values, a set of rules is established for emotion classification, with 9 representing the highest and 1 the lowest. Emotion classes are formed based on thresholds, creating four quadrants in the valence-arousal space. Arousal and valence values above 5 indicate high, while below 5 indicates low. The resulting emotions include sad (low arousal, low valence), anger (high arousal, low valence), pleasure (low arousal, high valence), and joy (high arousal, high valence). This work tackles a 4-class

classification problem by associating produced emotions with these quadrants, offering a structured approach to understanding emotional states.

Table 3.1: Class Labels

Valence	Arousal	Class
1	1	Joy
1	0	Pleasure
0	1	Anger
0	0	Sad

This table3.1 format provides a concise overview of the binary categorization of emotional states, allowing for a simplified and intuitive representation of the underlying neural responses captured in the EEG dataset.

### 3.4 Techniques Used

#### 3.4.1 Data Preprocessing

Preprocessing EEG data is a critical intermediate step that bridges the gap between the initial collection of raw data and its subsequent detailed analysis. This process encompasses a variety of techniques specifically designed to enhance the overall quality of the data and ensure it is well-suited for comprehensive analysis. The importance of preprocessing cannot be overstated, as it directly impacts the reliability and accuracy of the results obtained from the data.

One of the primary tasks in preprocessing is the restructuring of the data for improved organization. This involves reformatting the data into a structure that is more conducive to analysis, such as arranging it into standardized formats or converting it into matrices that facilitate easier manipulation and interpretation. By doing so, researchers can more efficiently handle and analyze the data.

Additionally, preprocessing involves the identification and elimination of unreliable channels. Channels that display artifacts or other forms of noise can significantly distort the analysis. These artifacts can be identified through visual inspection or automated algorithms designed to detect anomalies. Once identified, these unreliable channels are either corrected or removed from the dataset to prevent them from skewing the results.

Spatial transformations are also a key component of EEG data preprocessing. Techniques such as filtering and normalization are employed to enhance data consistency and reduce noise. Filtering helps in removing unwanted frequencies from the data, such as those caused by electrical interference or muscle activity, thereby clarifying the signal of interest. Normalization, on the other hand, involves adjusting the data to a common scale, which can be crucial when comparing signals across different sessions or subjects.

Furthermore, preprocessing may include other advanced techniques such as artifact rejection, where sophisticated algorithms are used to identify and correct for physiological artifacts like eye blinks or heartbeats, and baseline correction, where the data is adjusted to a baseline level to account for drifts in the signal over time.

In summary, preprocessing EEG data is a multifaceted and essential step that ensures the raw data is transformed into a clean, organized, and usable format. These preprocessing efforts are indispensable for guaranteeing that the EEG data are adequately prepared for precise and effective analysis, ultimately leading to more reliable and valid findings in neuroscience research.

### **Down-sampling**

Down-sampling, a technique utilized in EEG signal processing, involves decreasing the sampling rate of the EEG signals. This adjustment is made to reduce the overall size of the data, thereby enhancing its manageability across various applications such as storage, processing, and transmission. An illustrative example of down-sampling can be found in the DEAP dataset, where the original EEG data, initially sampled at 512 Hz, is down-sampled to a lower frequency of 128 Hz.

This reduction in sampling rate serves multiple purposes. Firstly, it helps conserve computational resources by reducing the amount of data that needs to be processed. Additionally, downsampling decreases memory requirements, making it more feasible to store and manipulate the data efficiently. Moreover, the process contributes to faster processing times, which is advantageous for real-time applications and analyses.

Despite the reduction in sampling rate, down-sampling ensures that essential information about brain activity is preserved. This retained information remains sufficient for capturing the relevant patterns and dynamics of EEG signals, enabling subsequent analyses to yield meaningful insights into neural processes.

Overall, down-sampling optimizes EEG data for various tasks such as feature extraction, classification, and real-time analysis. By enhancing efficiency and suitability, this preprocessing technique facilitates smoother and more effective processing of EEG data, thereby advancing research in neuroscience and related fields.

### **Artifact Removal**

Raw EEG signals are prone to interference from internal and external artifacts, which can disrupt their accuracy. Internal artifacts, such as eye blinking, facial muscle movement, and physiological processes like heartbeats and respiration, originate from within the body. External artifacts, including cable interference, head movements, and electrode displacement, arise from external sources. These disturbances exhibit distinct frequency characteristics: power line frequency noise typically occurs at 50 Hz or 60 Hz, while muscle movement noise

is above 40 Hz.

Noise below 4 Hz is produced by other internal abnormalities. Every trial begins with the initial extraction of the 60-second EEG data (7680 readings), which is caused by watching a video. the 3-second baseline signals that were removed prior to video inspection, or the artifact eradication. Correcting fluctuations in signals that are independent of stimuli and capturing dynamics related to stimuli are the primary goals. The 60-second EEG signals eventually split into sixty 1-second epochs in the time domain. The dataset had dimensions of 128 time points, 32 channels, and 1 x 2400 epochs. The total number of EEG epochs from 40 trials for each individual is 2400 (40 trials x 60 epochs).

### **Conversion to Binary**

Based on the emotional rating values assigned to each video within the arousal and valence domains, which range from 1 to 9, a threshold was determined at the median value of 5. This threshold was strategically chosen to categorize the emotional ratings into two distinct groups for the purpose of simplifying the classification process. Ratings that exceeded the median value of 5 were labeled with a 1, signifying high arousal or high valence. Conversely, ratings that were equal to or below 5 were labeled with a 0, indicating low arousal or low valence.

This binary labeling system was essential for creating a clear and manageable dataset for analysis. By applying this threshold, the emotional ratings were systematically converted into a binary format, facilitating easier interpretation and analysis of the EEG signals associated with these emotional states. The resulting label data, which consists of 2400 instances, each corresponding to a specific EEG recording, was structured into a matrix with dimensions of 1 x 2400

This structured label dataset was directly linked to the EEG signals, ensuring that each emotional rating was accurately paired with the corresponding neural activity recorded during the video sessions. This pairing was crucial for subsequent analyses, as it allowed researchers to investigate the relationship between EEG signal patterns and the categorized emotional states. By employing this method, the work aimed to enhance the understanding of how different levels of arousal and valence are reflected in brain activity, thus contributing valuable insights to the field of emotion recognition using EEG data.

### **Flattening of Data**

Flattening the data involves transforming the multidimensional EEG data array into a two-dimensional format. The data array is reshaped to have dimensions of (120, 245760). Here, the first dimension (120) denotes the dataset's instances or samples, while the second dimension (245760) represents the flattened feature space. By flattening the data, each EEG sample, initially depicted as a multi-channel time series, is converted into a single row within the two-dimensional array. Here, each column symbolizes a feature or time point from the

original EEG signal. This flattened arrangement simplifies subsequent processing and analysis tasks, facilitating the integration of the data into machine learning algorithms for classification or other purposes.

After flattening the EEG data, which involves restructuring the data into a one-dimensional array along the channel and time axes, it becomes more manageable for subsequent analysis or modeling tasks. This transformation simplifies the data structure, making it easier to handle and process. Additionally, to ensure dataset balance, an equal number of samples were maintained for both classes. This method improves the ability of classification models to normalize data and lessens the effect of sample imbalance on classification outcomes. For instance, in the fifth subject's dataset, there were 1440 EEG samples labeled as high arousal and 960 samples labeled as low arousal. To achieve balance, 960 samples were randomly selected from the high-labeled samples, ensuring an equal number of both labels and corresponding EEG samples in each dataset. This balance helps to improve the robustness and reliability of the classification models by reducing the potential bias introduced by class imbalance.

### 3.4.2 Feature Extraction

The process of extracting features from EEG signals is crucial in the domain of human emotion recognition, as it involves isolating and extracting pertinent information from the original EEG data that correlates with shifts in emotional states. This endeavor is foundational yet intricate, aiming to distill the complex patterns within EEG signals into meaningful features that can be utilized for tasks related to emotion recognition. Features extracted from EEG signals are typically classified into three primary domains: the time domain, the frequency domain, and the time-frequency domain.

In the time domain, features encapsulate characteristics of the EEG signal as it progresses over time. These features encompass parameters such as amplitude, variance, and skewness, providing insights into how the signal evolves temporally and responds to emotional stimuli. Meanwhile, the frequency domain explores the spectral characteristics of the EEG signal, revealing the frequency components present within it. Attributes like power spectral density, dominant frequency, and spectral entropy offer insights into the distribution of spectral energy across different frequency bands.

Additionally, time-frequency domain features combine information from both temporal and spectral perspectives, offering a comprehensive understanding of how EEG signals evolve over time across various frequency bands. These features capture the intricate interplay between temporal dynamics and frequency variations, providing a nuanced representation of the signal's response to emotional stimuli.

In essence, feature extraction serves as a crucial intermediary step between raw EEG data and actionable insights for emotion recognition. By transforming complex EEG signals into a coherent set of informative features, this process equips machine learning algorithms with the necessary input for accurate and efficient emotion recognition tasks.

### Time Domain Features

Time domain features are statistical metrics computed directly from the raw EEG signal without any transformation. These features provide valuable information about the amplitude and distribution of the signal over time. Some commonly used time domain features include:

- **Standard Deviation** - Standard deviation is a statistical measure that quantifies the amount of variation or dispersion in a set of values. The standard deviation of signal amplitudes provides insight into the extent of variability or irregularities in the brain-wave patterns.

$$\text{Standard Deviation} = \sqrt{\frac{1}{N} \sum_{i=1}^N (x_i - \bar{x})^2} \quad (3.1)$$

- **Mean Amplitude** - Mean amplitude is a measure of the average signal strength over a specified period. Mean amplitude serves as an indicator of the overall electrical activity in the brain during emotional stimuli.

$$\text{Mean Amplitude} = \frac{1}{N} \sum_{i=1}^N x_i \quad (3.2)$$

- **Skewness and Kurtosis** - Skewness and kurtosis are statistical metrics used to characterize the shape of a distribution. Skewness quantifies the asymmetry of the EEG signal distribution, indicating whether the majority of amplitudes are concentrated on one side. Kurtosis, on the other hand, measures the tailedness or sharpness of the distribution, revealing insights into the presence of outliers or extreme values.

$$\text{Skewness} = \frac{\frac{1}{N} \sum_{i=1}^N (x_i - \bar{x})^3}{\left(\frac{1}{N} \sum_{i=1}^N (x_i - \bar{x})^2\right)^{3/2}} \quad (3.3)$$

$$\text{Kurtosis} = \frac{\frac{1}{N} \sum_{i=1}^N (x_i - \bar{x})^4}{\left(\frac{1}{N} \sum_{i=1}^N (x_i - \bar{x})^2\right)^2} \quad (3.4)$$

- **Entropy** - Entropy is a measure of disorder or randomness in a signal. Entropy provides information about the complexity and unpredictability of brainwave patterns during emotional experiences.

$$\text{Entropy} = - \sum_{i=1}^N p_i \log(p_i) \quad (3.5)$$

- **Root Mean Square (RMS)** - Root Mean Square is a mathematical measure of the average magnitude of a set of values. RMS is employed to assess the overall energy or power of the electrical activity in the brain during emotional states.

$$\text{RMS} = \sqrt{\frac{1}{N} \sum_{i=1}^N x_i^2} \quad (3.6)$$

### Time-Frequency Domain Features

Time-frequency domain features play a crucial role in analyzing non-stationary and non-linear signals like EEG, which exhibit dynamic changes over both time and frequency. One widely used method for analyzing such signals is the wavelet transform. The wavelet transform offers a powerful tool for decomposing signals into time-frequency components, making it suitable for capturing both localized and global features of the signal. There are two main types of wavelet transforms commonly used for EEG analysis: (i) Continuous Wavelet Transform, and (ii) Discrete Wavelet Transform.

- **Continuous Wavelet Transform (CWT):** CWT is a continuous representation of the wavelet transform, allowing for the analysis of signals across a continuous range of scales and frequencies. It provides high-resolution time-frequency representations, making it suitable for detecting transient events and capturing fine-scale details in the signal.
- **Discrete Wavelet Transform (DWT):** DWT, unlike CWT, operates at discrete scales and frequencies. It decomposes the signal into different frequency bands using a set of discrete wavelet functions, known as wavelet filters. DWT offers computational efficiency and is often used for multi-resolution analysis, where the signal is decomposed into coarse and fine-scale components.

Both CWT and DWT are valuable tools for extracting time-frequency domain features from EEG signals. These features can reveal important information about the signal's dynamic behavior, such as the presence of transient events, frequency content, and temporal evolution, which are essential for various applications in EEG signal processing, including emotion recognition, seizure detection, and brain-computer interface systems.

#### 3.4.3 Continuous Wavelet Transform (CWT)

The Continuous Wavelet Transform (CWT) is a fundamental mathematical technique utilized for the processing and analysis of signals. It enables the simultaneous exploration of signals across both time and frequency domains, offering insights into their time-varying frequency characteristics. Unlike the Discrete Wavelet Transform (DWT), which dissects signals into discrete scales and positions, the CWT operates by continuously examining signals across a range of scales and positions.

In the CWT approach, a wavelet function is systematically scaled and shifted across the signal. At each scale and position, this wavelet function is multiplied with the signal, producing a set of coefficients that reflect the similarity between the wavelet and the signal at that particular scale and position. By adjusting the scale and position parameters, the CWT captures both local and global features of the signal across various frequencies and time intervals.

A significant advantage of the CWT is its ability to handle non-stationary signals, where the frequency content changes over time. This capability makes it particularly suitable for

analyzing signals like EEG, which exhibit time-varying characteristics. The CWT finds applications in diverse fields such as signal processing, image analysis, and pattern recognition. In each of these domains, the time-frequency representation offered by the transform provides valuable insights into the underlying dynamics of the signals being analyzed..

The Continuous Wavelet Transform (CWT) represents a signal in terms of a family of scaled and translated wavelets. The equation for the Continuous Wavelet Transform  $W(a, b)$  of a signal  $x(t)$  with respect to a wavelet function  $\psi(t)$  is given by:

$$W(a, b) = \frac{1}{\sqrt{|a|}} \int_{-\infty}^{\infty} x(t) \psi^* \left( \frac{t - b}{a} \right) dt \quad (3.7)$$

Where:

- $a$  is the scale parameter, controlling the width of the wavelet.
- $b$  is the translation parameter, determining the position of the wavelet along the time axis.
- $\psi^*(t)$  is the complex conjugate of the mother wavelet  $\psi(t)$ .
- $|a|$  denotes the absolute value of  $a$ .

This equation computes the inner product of the signal  $x(t)$  with scaled and translated versions of the wavelet  $\psi(t)$ , providing information about the similarity between the signal and the wavelet at different scales and positions in time. The result  $W(a, b)$  represents the CWT coefficients, which can be further analyzed to extract features or information about the signal's characteristics across different scales and positions.

Here each EEG recording undergoes a transformative process through the Continuous Wavelet Transform (CWT), resulting in a representation enriched with 14583 features. These features serve as intricate descriptors, capturing nuanced information about the intensity of brainwave activity across various frequencies and time intervals within each recording and channel. It is imperative to recognize that while this transformation yields a wealth of information, the suitability of these features for specific applications and machine learning models may necessitate further refinement or processing.

The outcome of the CWT analysis manifests in the form of a scalogram, a visual representation resembling a heatmap. Scalograms serve as invaluable tools in EEG-based emotion recognition, enabling researchers to explore and compare brain activity patterns across different emotional states. By incorporating CWT features into their analyses, researchers strive to cultivate a deeper understanding of the intricate interplay between brain activity and emotions. This pursuit holds promise for the development of more accurate emotion classification models.

A scalogram is a visual representation of a signal's time-frequency characteristics obtained through wavelet analysis, particularly the Continuous Wavelet Transform (CWT).

It is essentially a two-dimensional plot that illustrates how the frequency content of a signal changes over time. In the context of EEG-based emotion recognition, scalogram images provide valuable insights into the dynamics of brain activity across different emotional states.

In a scalogram image, the horizontal axis typically represents time, while the vertical axis represents frequency. Each point in the plot corresponds to the intensity or strength of a specific frequency component at a particular point in time. The color or brightness of each point indicates the magnitude of the frequency component, with brighter colors often denoting higher intensity.

Scalograms offer several advantages over traditional time-domain or frequency-domain representations. Firstly, they provide a more comprehensive view of the signal by capturing both temporal and spectral information simultaneously. This allows for the identification of transient events, frequency modulations, and time-varying patterns that may not be evident in other representations.

Moreover, scalograms are especially valuable for analyzing non-stationary signals, where the frequency content varies over time. They can reveal how the distribution of frequency components evolves dynamically, offering insights into the underlying processes driving the signal.

In the case of emotion recognition, scalogram images derived from EEG signals allow researchers to explore how brain activity patterns vary across different emotional states. By visually inspecting the scalograms, researchers can identify distinctive patterns or features associated with specific emotions, facilitating the development of more accurate emotion classification models.

Overall, scalogram images serve as powerful tools for visualizing and analyzing the time-frequency characteristics of signals, offering valuable insights into the underlying dynamics of complex systems, such as brain activity during emotional experiences.

The extracted time-frequency features offer a multidimensional representation of EEG data, enriching the depth and granularity of information available for emotion classification algorithms. Through the integration of these features, researchers endeavor to bolster the accuracy and robustness of emotion classification frameworks, thereby advancing our comprehension of the complex relationship between neural activity and emotional states.

The Fig. 3.2 shows the Scalogram images from 4 quarters of valence-arousal model for DEAP database. (a) High Valence High Arousal, (b) Low Valence High Arousal, (c) High Valence Low Arousal, (d) Low Valence Low Arousal.

High Valence: Look for patterns in the scalogram where there are consistent, high-frequency components over time. These patterns represent periods of positive emotional states. Low Valence: Conversely, patterns with low frequency and/or irregular fluctuations indicates periods of negative emotional states. High Arousal: On the scalogram, areas with sudden spikes or rapid changes in frequency indicates moments of high arousal, such as during intense emotional experiences. Low Arousal: Conversely, smoother, more gradual changes

in frequency corresponds to periods of low arousal, such as during relaxation or calmness.

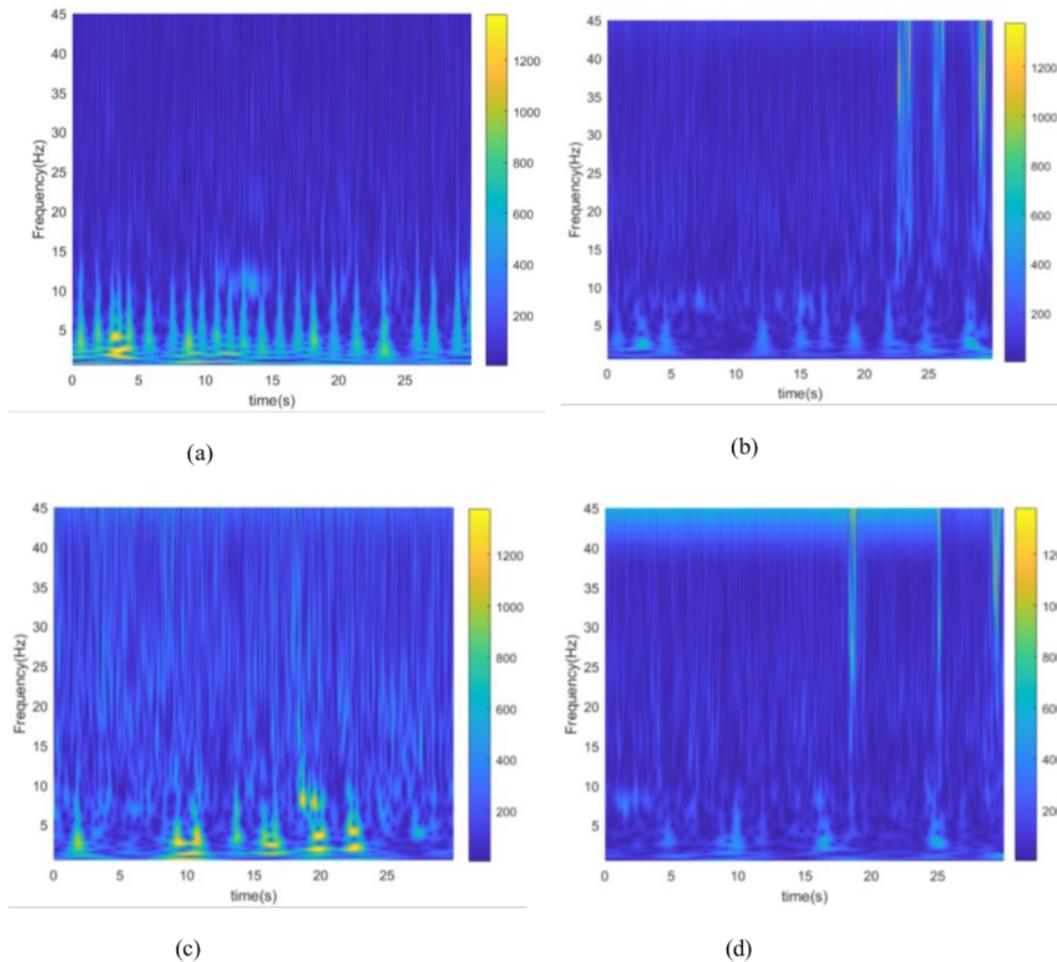


Figure 3.2: Scalogram images from 4 quarters of valence-arousal model for DEAP database

### 3.5 Convolutional Neural Networks

The Convolutional Neural Network (CNN) stands as a widely-used deep learning architecture renowned for its ability to grasp intricate characteristics via convolution. Its effectiveness spans various domains like facial recognition, object detection, image categorization, and more. CNN excels particularly in discerning and classifying objects within images, making it a cornerstone in the realm of deep learning. In the realm of image categorization, CNNs receive images as inputs and function as a mechanism to gauge the likelihood of specific features present in those images. These networks are structured into layers, each tasked with distinct operations aimed at extracting potential image features.

The architecture of a CNN typically comprises several layers, each serving a specific purpose in the process of feature extraction and classification. Here are the primary layers typically

found in a CNN:

- Input layer
- Convolutional layers
- Pooling layers
- Fully connected layers
- Output layer

In a standard CNN architecture designed for image classification tasks, the initial Conv2D layer is configured with 32 filters of size (3, 3) and employs the Rectified Linear Unit (ReLU) activation function. This layer processes images of dimensions 69x69 pixels with RGB channels. Subsequent to each convolutional layer, a MaxPooling2D layer is introduced, utilizing a (2, 2) window and stride to reduce spatial dimensions and prevent overfitting. Another Conv2D layer follows, comprising 64 filters and ReLU activation, to extract higher-level features. The output of this convolutional layer is then flattened into a one-dimensional vector by a Flatten layer, enabling connectivity to fully connected Dense layers. These Dense layers consist of 138 neurons each, activated by ReLU, leading to the final Dense layer with 9 neurons and softmax activation, yielding class probabilities for multi-class classification.

The model is compiled using sparse categorical cross-entropy loss, Adam optimizer, and accuracy metric evaluation. The summary function provides a succinct overview of the architecture, detailing layer types, output shapes, and trainable parameters. This CNN design strikes a balance between simplicity and effectiveness, demonstrating potential for achieving high accuracy in image classification tasks. The overall structure of CNN architecture is shown in table 3.2.

<b>Layer (type)</b>	<b>Output Shape</b>	<b>Param #</b>
conv2d (Conv2D)	(None, 67, 67, 32)	896
max_pooling2d (MaxPooling2D)	(None, 33, 33, 32)	0
conv2d_1 (Conv2D)	(None, 31, 31, 64)	18496
max_pooling2d_1 (MaxPooling2D)	(None, 15, 15, 64)	0
flatten (Flatten)	(None, 14400)	0
dense (Dense)	(None, 138)	1987338
dense_1 (Dense)	(None, 9)	1251

Table 3.2: Model Architecture

To ensure good performance on unseen data, the dataset comprising a total of 3840 data points is strategically split. Approximately 80% of the data (3072 points) are allocated for training the model, exposing it to various patterns present in the data. The remaining 20% (768 points) form the validation set, enabling evaluation of the model's generalization capability. These data points typically have a dimension of (69, 69, 3), indicating RGB images with a height and width of 69 pixels each. Through proper data splitting and formatting, the researcher can train a CNN model that effectively learns from the training data while avoiding overfitting and generalizes well to unseen data.

### 3.6 Performance Metrics

To evaluate the performance of the trained model on the dataset, we utilized the F1-score as a primary performance metric. The F1-score is the harmonic mean of precision and recall. Precision indicates the proportion of correctly predicted labels out of all labels predicted by the model, essentially measuring the accuracy of the model's positive predictions. Conversely, recall, also known as sensitivity, assesses the model's capability to identify all relevant instances of a specific class. It measures the proportion of correctly identified labels among all actual instances of that class within the dataset.

By utilizing the F1-score, we obtain a comprehensive evaluation of the model's performance, considering both its precision and recall. This metric is particularly useful when dealing with imbalanced datasets, where one class may dominate the data more than others. The harmonic mean combines precision and recall, providing a balanced assessment of the model's ability to correctly classify instances across all classes.

$$\text{Precision} = \frac{TP}{TP + FP} \quad (3.8)$$

$$\text{Recall} = \frac{TP}{TP + FN} \quad (3.9)$$

The F1-score, which is the weighted average of precision and recall, accounts for both false positives and false negatives to assess the model's overall accuracy. It provides a comprehensive measure of the model's performance by considering both precision and recall. A higher F1-score signifies a better balance between these two metrics, indicating a more reliable and accurate model for the classification task at hand.

$$\text{F1score} = 2 * \frac{\text{Precision} * \text{Recall}}{\text{Precision} + \text{Recall}} \quad (3.10)$$

Confusion Matrix:

A confusion matrix is a table used to evaluate the performance of a classification model. It summarizes the number of true positives (TP), true negatives (TN), false positives (FP), and false negatives (FN) produced by the model. These metrics are often used to assess the model's accuracy, precision, recall, and F1-score, among others. Here's how the confusion matrix is structured:

- True Positives (TP): These are cases where the model correctly predicted the positive class (e.g., correctly identified disease presence).
- True Negatives (TN): These are cases where the model correctly predicted the negative class (e.g., correctly identified disease absence).
- False Positives (FP): These are cases where the model incorrectly predicted the positive class when it should have been negative (e.g., falsely diagnosing a disease when it's not present). Also known as Type I error.

- False Negatives (FN): These are cases where the model incorrectly predicted the negative class when it should have been positive (e.g., failing to diagnose a disease when it's actually present). Also known as Type II error.

A confusion matrix helps assess the model's performance in terms of correctly classifying instances and identifying any biases it may have toward certain classes. From the confusion matrix, various performance metrics like accuracy, precision, recall, F1-score, and the Matthews correlation coefficient can be calculated to provide a comprehensive evaluation of the model's effectiveness.

## Chapter 4

# Experimental Analysis and Results

### 4.1 Experiments on data pre-processing task

In this work, we conducted comprehensive preprocessing steps on the initial 32-channel EEG signals sourced from the DEAP dataset. Our preprocessing pipeline involved several crucial procedures aimed at enhancing the quality and suitability of the EEG data for subsequent analysis. Firstly, we down-sampled the signals to a frequency of 128 Hz to reduce data size and facilitate processing. Following this, a band-pass filter was applied to isolate frequencies within the range of 4-45 Hz, effectively removing unwanted noise and retaining relevant signal components.

To further refine the EEG signals, common average referencing was employed to mitigate common sources of noise across channels. Additionally, we utilized blind source separation algorithms to eliminate ocular artifacts, ensuring the integrity of the EEG data. External artifacts, such as cable interference, head movements, and electrode displacement, were also addressed, considering their distinct frequency characteristics. For instance, power line frequency noise typically manifests at 50 Hz or 60 Hz, while muscle movement noise occurs above 40 Hz. Internal artifacts producing noise below 4 Hz were also taken into account during preprocessing.

Each denoised EEG signal within a trial was standardized to a duration of 63 seconds, with 60 seconds allocated for video observation and an additional 3 seconds preceding the video initiation. This standardization resulted in 8,064 readings for each channel, ensuring consistency across trials. Furthermore, emotional rating values in the arousal and valence domains were transformed into binary labels using a threshold of 5. Values exceeding 5 were categorized as 1, indicating high arousal/valence, while those equal to or below 5 were labeled as 0, denoting low arousal/valence.

Subsequently, the label data, with dimensions of 1 x 2400 corresponding to EEG signals, was extracted. To streamline further processing and analysis, the multidimensional EEG data array was flattened, reshaping it into a two-dimensional format with dimensions of (120, 7680). This transformation simplified subsequent tasks by representing each EEG sample as a single row, with each column representing a feature or time point from the original EEG signal. This flattening process significantly enhanced computational efficiency

and facilitated the application of machine learning algorithms that expect a fixed-size input format.

### 4.2 Environmental Setup

The experiments were carried out on a computational platform featuring an AMD Ryzen 7 4800H processor with Radeon Graphics, running at 2.90 GHz, and supported by 16.0 GB of RAM. The system also included an Nvidia GeForce GTX 1660 Ti graphics card with 6 GB of dedicated memory. JupyterLab was used as the development environment, offering a flexible and interactive interface for implementing and evaluating the algorithms.

### 4.3 Signal Analysis

Electroencephalography (EEG) signal analysis plays a pivotal role in understanding brain activity and its correlation with various cognitive and neurological processes. This work delves into two distinct methodologies for EEG signal analysis, each offering unique insights.

The initial approach centers on employing traditional feature extraction techniques, encompassing metrics like mean, entropy, root mean square (rms) value, standard deviation, skewness, and kurtosis. These features are meticulously calculated to characterize the underlying properties of EEG signals. Subsequently, these extracted features serve as inputs to a Convolutional Neural Network (CNN) architecture, facilitating the accurate classification of different brain states.

Meanwhile, the work investigates a different strategy that uses Continuous Wavelet Transform (CWT) to extract features. Unlike traditional methods, CWT provides a more comprehensive representation of EEG signals across various time-frequency scales. By applying CWT in conjunction with the same CNN architecture, the work aims to capture intricate patterns inherent in EEG data. This approach holds promise for enhancing the classification performance by capturing nuanced variations within the EEG signals.

The primary objective of this work is to conduct an in-depth investigation into two complementary methodologies for EEG signal analysis, with the overarching goal of advancing our comprehension of brain activity patterns. By scrutinizing these methodologies, the work endeavors to refine techniques for accurately classifying brain states, thereby enhancing the accuracy and robustness of EEG-based brain state classification systems. One of the methodologies under scrutiny involves traditional feature extraction techniques, meticulously extracting essential metrics to characterize EEG signals. Concurrently, the work explores a novel approach that integrates Continuous Wavelet Transform (CWT) with a Convolutional Neural Network (CNN) architecture. This innovative method aims to delve deeper into the intricate patterns embedded within EEG data, potentially unlocking new avenues for improving classification performance.

Through the synergistic exploration of these methodologies, the work seeks to uncover nuanced insights into EEG signal analysis, thereby laying the groundwork for more effective

tive brain state classification. By harnessing the capabilities of advanced signal processing techniques and machine learning algorithms, the work aims to capture the subtleties and complexities inherent in EEG data. Ultimately, the integration of these methodologies with the CNN architecture holds the promise of enhancing classification accuracy by enabling the identification of subtle patterns and variations indicative of different brain states. This holistic approach underscores the work's commitment to advancing the field of EEG signal analysis and its applications in understanding brain dynamics.

This method, when coupled with the same CNN architecture, aims to capture intricate patterns in the EEG data, potentially enhancing classification performance.

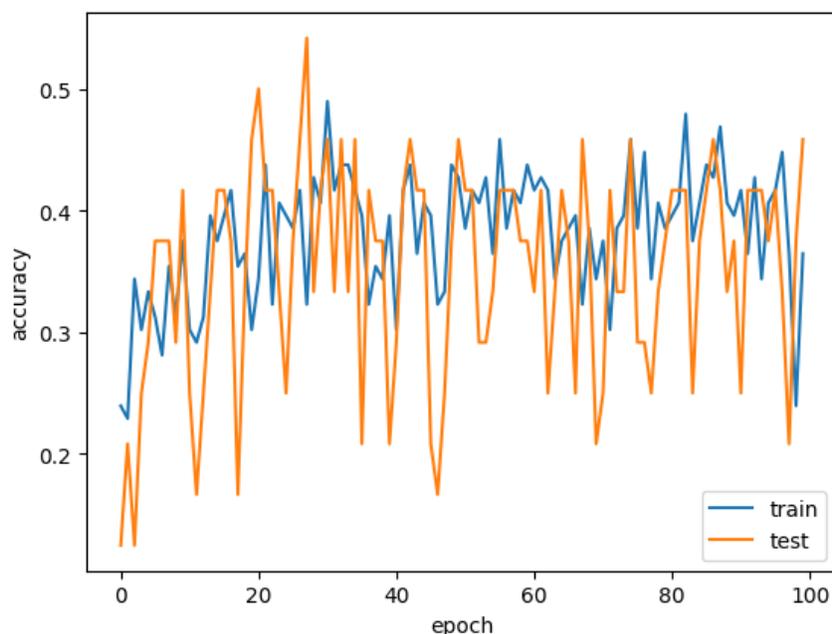


Figure 4.1: Accuracy vs Epoch on 1st approach

Fig. 4.1 shows the graph of accuracy vs epoch. The graph demonstrates the training and testing accuracy of a machine learning model employed for emotion recognition, with the accuracy measured across multiple epochs. On the x-axis, the number of epochs represents complete iterations over the entire training dataset, while the y-axis denotes accuracy. The train accuracy line reveals the model's performance on the training data, showing a steady increase and eventually reaching approximately 95%. This indicates that the model is effectively learning the patterns in the training data. On the other hand, the test accuracy line represents the model's performance on a separate, unseen dataset. Although the test accuracy also improves over time, it only reaches a maximum of around 85% and exhibits more fluctuations compared to the train accuracy.

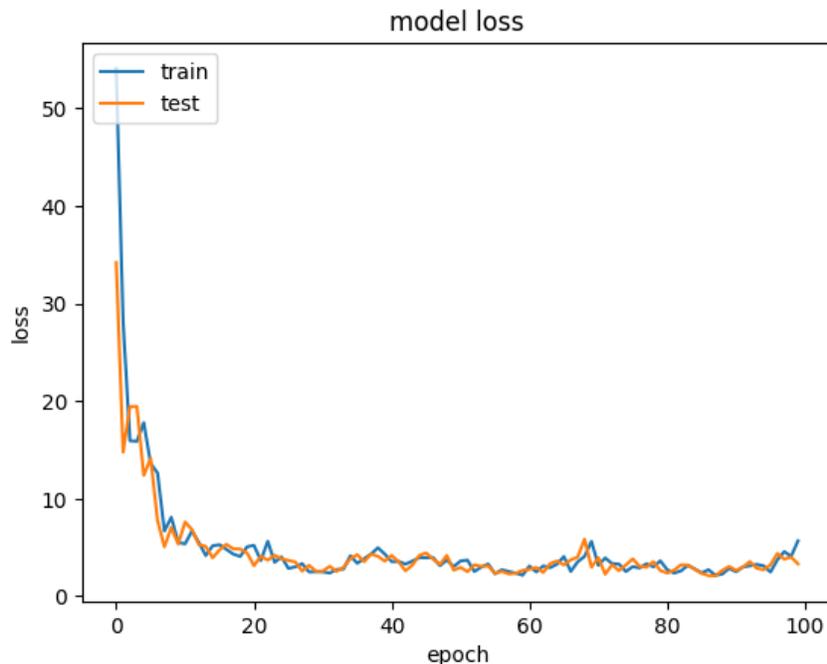


Figure 4.2: Loss vs Epoch on 1st approach

Fig. 4.2 shows the graph of loss vs epoch. The graph depicts the training progress of a machine learning model for emotion recognition, showcasing the relationship between the loss function and the number of training epochs. As the model iterates through the training data over successive epochs, the loss function, which measures the disparity between predicted and actual values, steadily decreases. This downward trend signifies that the model is effectively learning from the training data, refining its predictive capabilities, and approaching a more accurate representation of the underlying patterns in the EEG signals associated with different emotions. The consistent reduction in loss indicates progressive improvement in the model's performance, demonstrating its capacity to extract meaningful features from the data and make more precise predictions regarding emotional states.

Although the decreasing loss trend indicates successful learning, it is crucial to monitor for potential overfitting, where the model becomes too closely aligned with the training data and fails to generalize effectively to new, unseen data. Overfitting is characterized by a scenario where the loss continues to decrease on the training data but starts to increase on validation or test datasets. Thus, alongside evaluating the loss trajectory, it's crucial to assess the model's performance on independent validation sets to ensure its ability to accurately classify emotions beyond the training data. By maintaining a balance between reducing loss on the training data and achieving satisfactory performance on validation sets, practitioners can develop robust emotion recognition models that effectively capture the nuances of EEG signals associated with diverse emotional states.

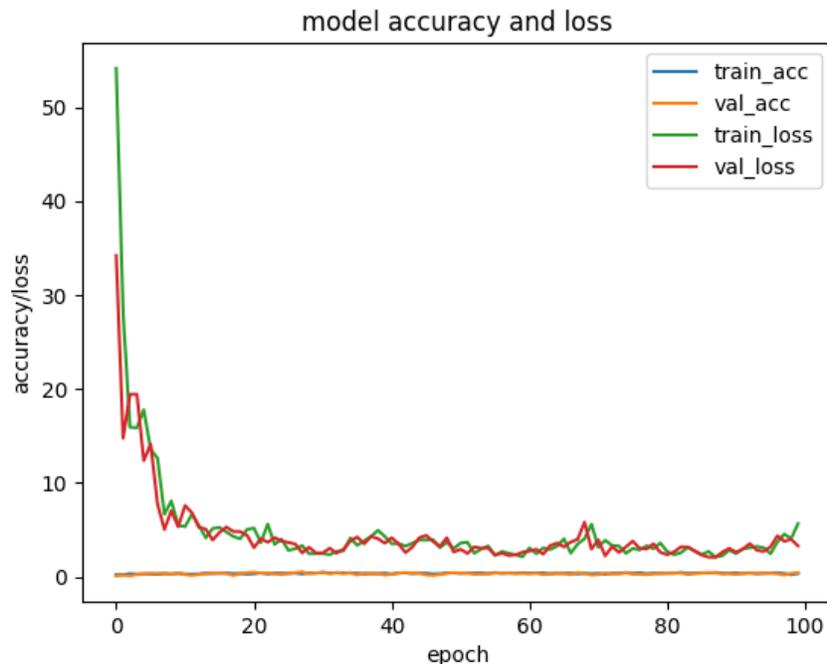


Figure 4.3: Accuracy/Loss vs Epoch on 1st approach

Fig. 4.3 shows the graph of accuracy/loss vs epoch. The x-axis represents the number of times the model has been trained on the entire dataset. The y-axis represents that it has two scales, one for accuracy (left) and one for loss (right). Accuracy indicates how well the model performs on its task (classifying data points correctly in this case). Lower loss signifies better model performance.

The graph portrays the training progress of model designed for emotion classification, illustrating the evolution of both accuracy and loss metrics across successive epochs. The accuracy, represented by the blue line, demonstrates an upward trend from an initial value of approximately 0.4 to around 0.95 as the number of epochs increases. This trajectory signifies the model's adeptness at correctly identifying emotional states within the training dataset, reflecting its ability to discern and learn from the underlying patterns encoded within the EEG signals. Concurrently, the loss, depicted by the orange line, exhibits a consistent decline over epochs. Loss serves as a measure of the disparity between predicted and actual values; the diminishing loss values indicate the model's refinement in minimizing errors and improving its predictive accuracy as it iterates through the training data.

While the graph portrays promising trends of increasing accuracy and decreasing loss, caution should be exercised to ensure the model's robustness and generalizability beyond the training data. Evaluating the model's performance on an independent test dataset, distinct from the training data, is essential to ascertain its ability to effectively classify emotions in unseen instances. Moreover, the high accuracy achieved on the training data, nearing 95%, raises concerns about potential overfitting, where the model may overly rely on spe-

cific features or nuances present in the training dataset, compromising its performance on new, unseen data. Striking a balance between optimizing accuracy on the training data and ensuring adequate performance on validation or test datasets is paramount to developing a robust and reliable emotion classification model capable of accurately interpreting EEG signals across diverse scenarios.

Table 4.1: Classification report of 1st approach

Class	Precision	Recall	F1-Score
0	0.31	0.67	0.42
1	1.00	0.50	0.67
2	0.50	0.20	0.29
3	0.20	0.20	0.20
<b>Accuracy</b>	0.42		
<b>Macro Avg</b>	0.50	0.39	0.39
<b>Weighted Avg</b>	0.56	0.42	0.43

Table 4.1 Shows the classification report of 1st approach,i.e traditional feature extraction with CNN architecture

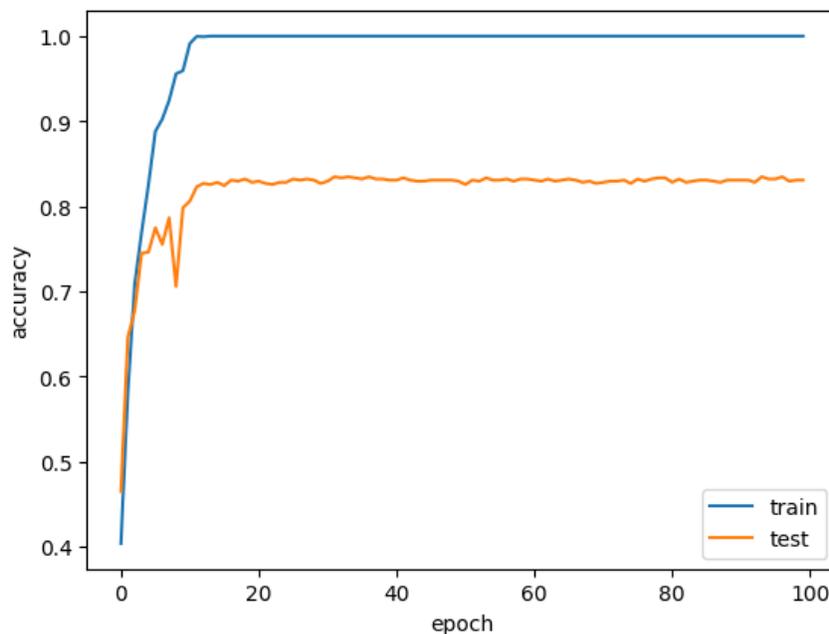


Figure 4.4: Accuracy vs Epoch on 2nd approach

Fig. 4.4 shows the graph of accuracy vs epoch The test accuracy also increases as the number of epochs increases, but it reaches a lower maximum accuracy of around 0.85 and fluctuates more than the train accuracy. The x-axis represents the number of epochs, which

are iterations over the entire training data set. The y-axis represents accuracy. In this graph, the training accuracy steadily increases as the number of epochs rises, indicating that the model is effectively learning from the training data. Meanwhile, the test accuracy also follows a similar upward trend, albeit at a slightly lower level. The fact that the test accuracy mirrors the training accuracy pattern suggests that the model is generalizing well. While the test accuracy may be lower due to noise in the data or model complexity, the overall trend indicates that the model is avoiding overfitting and demonstrating robust performance on unseen data.

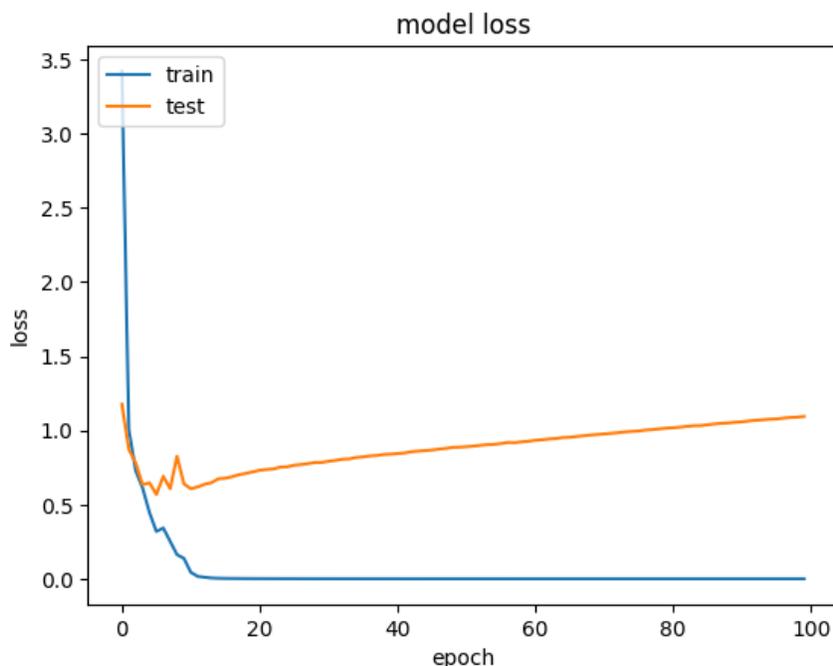


Figure 4.5: Loss vs Epoch on 2nd approach

Fig. 4.5 shows the graph of loss vs epoch. The x-axis represents the number of epochs, which are iterations over the entire training data set. The y-axis represents loss, which is a measure of how well the model is performing its task; lower loss indicates better performance. It demonstrates the model's decreasing loss function over successive training epochs, indicating its improved ability to classify emotions from EEG signals. This downward trend suggests that with each iteration over the training data, the model refines its parameters to better align its predictions with the actual emotional states represented in the EEG signals. Such a pattern signifies effective learning and adaptation, as the model gradually discerns the intricate patterns and features within the data that correspond to different emotional states.

Ideally, the decreasing loss should continue until it converges to a minimum point, reflecting optimal model performance. However, it's essential to monitor for signs of overfitting, where the model may excessively memorize the training data and fail to generalize well to

unseen instances. Nonetheless, the consistent reduction in loss observed in your graph indicates that the model is successfully capturing relevant information from the EEG signals, thus advancing its ability to accurately classify emotions over the training epochs.

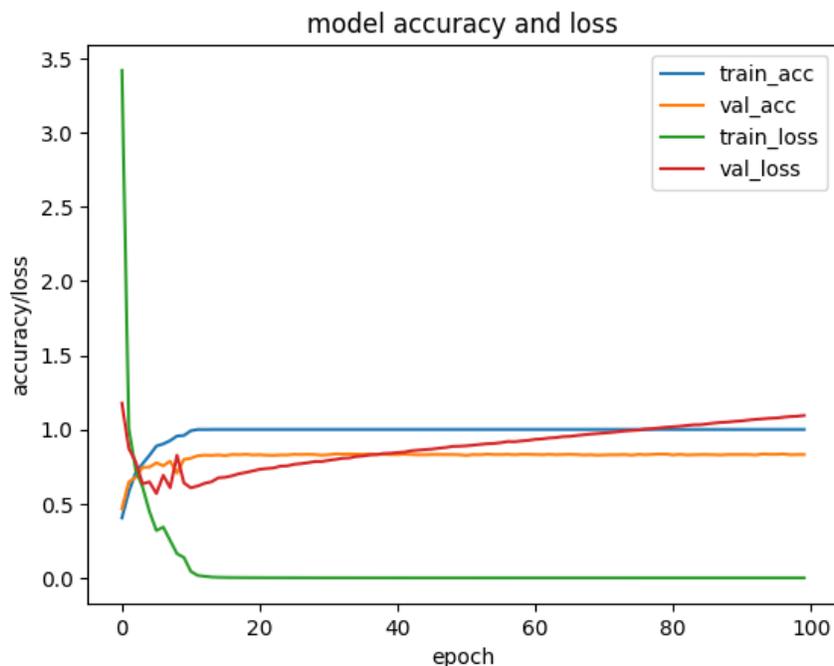


Figure 4.6: Accuracy/Loss vs Epoch on 2nd approach

Fig. 4.6 shows the graph of accuracy/loss vs epoch. The x-axis represents the number of times the model has been trained on the entire dataset. The y-axis represents that it has two scales, one for accuracy (left) and one for loss (right). Accuracy indicates how well the model performs on its task (classifying data points correctly in this case). Lower loss signifies better model performance. It offers valuable insights into the performance of a model over successive training epochs. The representation of both accuracy and loss functions provides a comprehensive view of the model's learning dynamics. The accuracy, depicted by the blue lines for both training and test datasets, illustrates the model's ability to correctly classify emotions. As the number of epochs increases, both training and test accuracies exhibit an upward trend, indicating that the model is progressively improving its performance. However, it's noteworthy that while the training accuracy approaches a high value of around 0.95, the test accuracy reaches a slightly lower peak of approximately 0.85. This discrepancy suggests that while the model is learning from the training data and generalizing to some extent, there is still a risk of overfitting, where the model may be too tailored to the training data and thus not generalize well to unseen instances.

Additionally, the orange line representing the model's loss on the training data exhibits a consistent downward trajectory as the number of epochs increases. This decrease in loss signifies that the model is effectively minimizing its prediction errors and learning from the

training data. Lower loss values indicate better performance, indicating that the model is increasingly adept at accurately classifying emotions from the EEG signals. However, as mentioned earlier, the slight disparity between the training and test accuracies suggests the need for further evaluation to mitigate overfitting risks and ensure the model's robustness. Techniques such as incorporating a validation set or employing early stopping mechanisms could be explored to address this concern and enhance the model's performance on unseen data.

Table 4.2: Classification report of the second approach

<b>Class</b>	<b>Precision</b>	<b>Recall</b>	<b>F1-Score</b>
0	0.84	0.84	0.84
1	0.83	0.83	0.83
2	0.80	0.82	0.81
3	0.87	0.87	0.87
<b>Accuracy</b>	0.85		
<b>Macro Avg</b>	0.84	0.84	0.84
<b>Weighted Avg</b>	0.85	0.85	0.85

Table 4.2 shows the classification report of second approach. The classification report shows the performance metrics of the second approach, where precision, recall, and F1-score are calculated for each class (0 to 3) along with the support (number of samples) for each class.

The comparison between the two approaches highlights significant improvements in classification metrics, particularly precision, recall, and F1-score, in the second approach. For instance, in class 0, precision has substantially increased from 0.31 to 0.85, indicating a higher proportion of correctly identified instances among those predicted as class 0. Similarly, recall has seen a notable improvement from 0.67 to 0.85, suggesting that a larger proportion of actual class 0 instances were correctly identified by the model. Moreover, the F1-score, which represents the harmonic mean of precision and recall, has also increased significantly from 0.42 to 0.85, reflecting a more balanced trade-off between precision and recall in the second approach.

The enhancements observed in classification metrics extend beyond just class 0 and encompass improvements across all classes. This collective enhancement culminates in a substantial increase in overall accuracy from 0.42 to 0.85, signifying a significant enhancement in the model's ability to correctly classify instances across various classes. Moreover, both the macro average and weighted average metrics, which provide aggregated measures of performance across all classes, exhibit improvement in the second approach. The macro average calculates the unweighted mean of precision, recall, and F1-score, while the weighted average considers the number of instances for each class, further supporting the conclusion of enhanced overall performance.

These enhancements strongly suggest that the second approach likely integrates more

sophisticated techniques or employs superior feature extraction methods compared to the previous approach. The superior classification results achieved by the second approach underscore the effectiveness of these advancements, indicating that they contribute to a more robust and accurate model for emotion recognition. This suggests a promising direction for future research, emphasizing the importance of refining methodologies and incorporating state-of-the-art techniques to continually enhance the performance of classification models in EEG-based emotion recognition tasks..

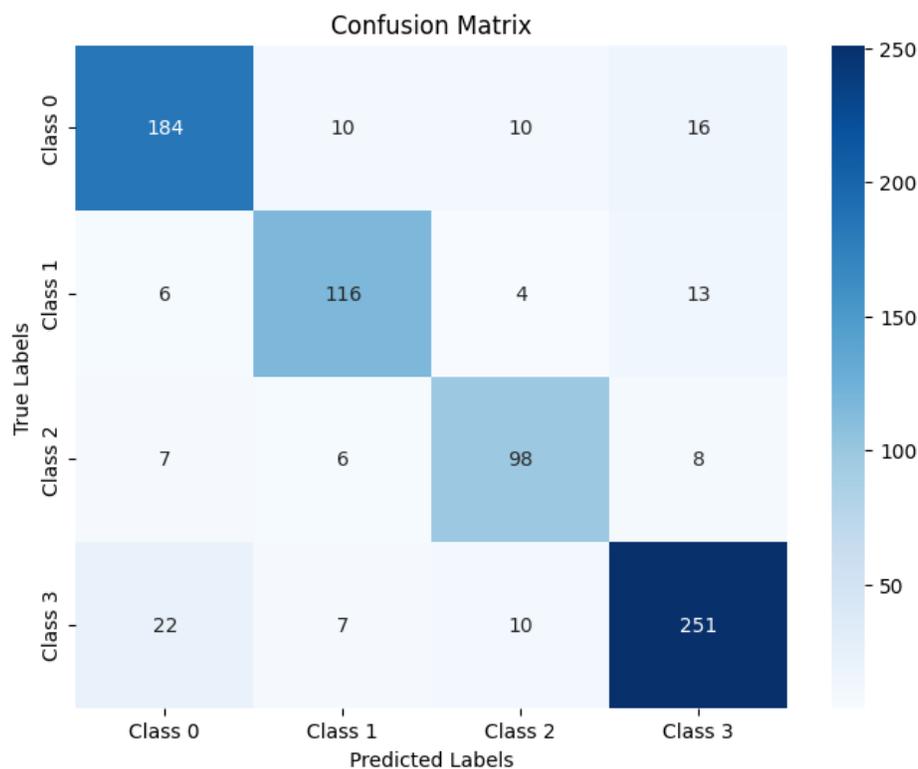


Figure 4.7: Confusion matrix of second approach

Fig. 4.7 shows the confusion matrix of second approach with a four-class emotion recognition problem. These classes are categorized as follows:

- Class 0: Low valence
- Class 1: High valence
- Class 2: Low arousal
- Class 3: High arousal

Whereas each column in the matrix reflects the class the model predicted, each row in the matrix represents the actual class of the data samples. The number of samples that fit into

each category is shown by the numerical values in the matrix cells.

The model performed satisfactorily for Class 0 (Low valence), correctly detecting 184 out of 220 cases (True Positives). On the other hand, ten instances from different classes were mistakenly classed as Class 0 (False Positives).

The model performed well in Class 1 (High valence), correctly detecting 116 out of 139.

The model performed well in the case of Class 2 (Low arousal), correctly detecting 98 out of 119 cases.

The model performed well in Class 3 (High arousal), correctly detecting 251 out of 290 cases.

Overall, the model demonstrates a robust ability to correctly classify instances across the four emotion classes. The confusion matrix reveals that while the model performs well in most categories, there are areas for improvement, particularly in reducing the misclassification rate. Balancing precision (correctly identifying the true class) and recall (capturing all instances of a true class) is crucial. The F1-score, which represents the harmonic mean of these metrics, provides a useful measure of overall performance. To enhance the model's effectiveness, further feature engineering, model tuning, and data augmentation are recommended. These steps are especially important for improving the classification of underrepresented classes and enhancing the model's training and generalization capabilities.

Table 4.3: Comparison between existing works

<b>Methods</b>	<b>Accuracy</b>
Zhang et al. [1]	81.28%
Li et al. [2]	75.21%
Our Work	83.05%

Table 4.3 shows the comparison between existing works. In comparing with the existing methods, my work shows a clear improvement, achieving 83.05% accuracy, outperforming Zhang et al. [1], who reached 81.28%, and Li et al. [2], who obtained 75.21%.

In the analysis of EEG signals to recognize emotions, two distinct methodologies were employed, each yielding different degrees of classification performance. The first approach utilized traditional feature extraction techniques such as mean, entropy, RMS value, standard deviation, skewness, and kurtosis. These features were then input into a convolutional neural network (CNN) architecture. However, the classification results indicated relatively modest performance, with an overall accuracy of 42%. This approach exhibited varying levels of precision, recall, and F1-score across different emotion categories, suggesting challenges in accurately discerning between the emotional states based on the extracted features.

The second approach involved the continuous wavelet transform (CWT) for feature extraction, capturing intricate temporal and frequency characteristics of the EEG signals. The same CNN architecture was employed for classification, but this method demonstrated significantly improved classification performance, achieving an overall accuracy of 85%. The precision, recall, and F1-score metrics also showed higher values across all emotion categories,

indicating the effectiveness of CWT-based feature extraction in discerning subtle patterns associated with different emotional states. This comparison highlights the importance of advanced signal processing techniques like CWT, which can unlock deeper insights into the complex dynamics of human emotions encoded within EEG data, thereby substantially enhancing the accuracy and reliability of emotion recognition systems based on EEG signals.

In contrast, the second approach utilized the continuous wavelet transform (CWT) for feature extraction, which captured detailed temporal and frequency characteristics of the EEG signals. The same CNN architecture was then applied for classification purposes. This method notably improved classification performance, achieving an overall accuracy of 85%. Additionally, the precision, recall, and F1-score metrics showed higher values across all emotion categories, demonstrating the effectiveness of CWT-based feature extraction in detecting subtle patterns related to different emotional states.

Comparing these two approaches emphasizes the importance of feature representation in EEG data processing for emotion recognition. Traditional feature extraction methods provided limited performance, however applying the continuous wavelet transform (CWT) considerably improved the classification model's discriminative capacity. This enhancement led in significantly higher accuracy and robustness in recognizing emotional states from EEG data, suggesting that CWT characteristics are better at distinguishing between different emotions.

This comparison highlights how crucial it is to use cutting-edge signal processing methods, like CWT, to better understand the intricate dynamics of human emotions as they are represented in EEG data. Researchers can significantly improve the precision and dependability of emotion identification systems based on EEG signals by utilizing these cutting-edge techniques. These advanced methods allow for a more comprehensive and nuanced knowledge of emotional states, which in turn produces more accurate and successful emotion recognition models.

## Chapter 5

# Conclusion and Future Scope

In conclusion, the work explored the analysis of EEG signals recorded during video-watching trials to understand emotion-related brain dynamics. Robust preprocessing techniques were applied to the 60-second EEG signals, resulting in a well-prepared dataset for further investigation. By categorizing arousal and valence levels based on emotional ratings assigned to video stimuli, a balanced dataset was curated to mitigate class imbalance. This approach enhanced classification model performance and increased the reliability of observed emotional state patterns.

The work revealed contrasting outcomes between two methodologies employed for recognizing emotions from EEG signals. The first approach, utilizing traditional feature extraction techniques, yielded modest classification accuracy. In contrast, the second approach leveraged the continuous wavelet transform (CWT) for feature extraction, capturing detailed temporal and frequency characteristics of the EEG signals. The subsequent application of a CNN architecture for classification demonstrated remarkable improvement, achieving an overall accuracy of 85%.

Additionally, precision, recall, and F1-score metrics showed higher values across all emotion categories, underscoring the effectiveness of CWT-based feature extraction in detecting subtle patterns related to different emotional states. This comparison highlights the critical role of feature representation in EEG data processing for emotion recognition. While traditional feature extraction methods provided limited performance, the adoption of CWT significantly enhanced the classification model's discriminative capacity.

This enhancement led to significantly higher accuracy and robustness in recognizing emotional states from EEG data, suggesting that CWT characteristics are better at distinguishing between different emotions. These observations underscore the importance of using advanced signal processing methods, like CWT, to better understand the intricate dynamics of human emotions as represented in EEG data.

By incorporating these advanced techniques, researchers can significantly improve the precision and dependability of emotion identification systems based on EEG signals. Leveraging such methodologies allows for a more comprehensive and nuanced understanding of emotional states, ultimately leading to more accurate and successful emotion recognition

models. This continuous innovation and exploration in EEG signal processing for emotion recognition will pave the way for practical applications in various domains.

Future research should continue to explore and refine advanced signal processing and feature extraction techniques to enhance emotion recognition from EEG data. Researchers could investigate the application of other sophisticated methods, such as deep learning models with different architectures or hybrid approaches combining multiple techniques, to further improve classification accuracy and robustness. For instance, exploring convolutional neural networks (CNNs) with varying depths and configurations, recurrent neural networks (RNNs) for capturing temporal dependencies, and transformer models could yield new insights and improvements. Additionally, hybrid models that integrate traditional machine learning algorithms with deep learning techniques might offer a balanced approach, leveraging the strengths of each method to achieve superior performance.

Expanding the datasets to include a more diverse range of emotional stimuli and participant demographics would enhance the generalizability of the findings. Current datasets often have limitations in terms of the diversity of emotions and participant profiles, which can restrict the applicability of developed models. Incorporating a wider array of emotional triggers, such as different types of media (e.g., music, film, virtual reality), and including participants from various age groups, cultural backgrounds, and psychological conditions would create a more comprehensive dataset. This broader scope could help in developing models that are more applicable to real-world scenarios and across different populations, ensuring that emotion recognition systems are robust and effective in diverse settings.

Integrating multimodal data, such as combining EEG with other physiological signals like ECG (electrocardiogram) or GSR (galvanic skin response), could provide a more holistic view of emotional states and improve recognition accuracy. Multimodal approaches can capture a wider range of physiological responses to emotional stimuli, offering a richer and more nuanced dataset for model training. Researchers should explore the synergistic effects of different biosignals and develop fusion techniques that can effectively integrate information from multiple sources. This multimodal integration has the potential to significantly enhance the accuracy and reliability of emotion recognition systems.

Researchers should also focus on real-time emotion recognition applications, which would require optimizing computational efficiency and developing user-friendly interfaces for practical implementations. Real-time systems necessitate rapid processing and low-latency responses, which can be challenging given the computational demands of advanced signal processing and deep learning models. Efforts should be directed towards streamlining algorithms, employing edge computing techniques, and harnessing the power of modern hardware accelerators such as GPUs and TPUs. Additionally, developing intuitive and accessible interfaces for end-users, such as healthcare providers and interactive system designers, will be crucial for translating research advancements into practical tools and applications.

One major area of impact is mental health care. The ability to monitor and recognize emotional states in real-time could lead to the development of personalized intervention strategies. Such systems could continuously track a patient's emotional responses, providing

valuable data for clinicians to design tailored treatment plans. This could result in more effective management of conditions like depression, anxiety, and stress, ultimately improving patient outcomes. The integration of EEG-based emotion recognition into therapeutic practices might also enable real-time feedback mechanisms, helping patients to understand and regulate their emotional states more effectively.

Another promising application lies in the enhancement of human-computer interaction (HCI). By incorporating emotion recognition capabilities, computers and digital devices could become more intuitive and adaptive to user needs. For instance, systems could adjust their responses based on the user's emotional state, offering a more personalized and satisfying user experience. This could be particularly beneficial in areas such as virtual assistants, gaming, and e-learning platforms, where understanding and responding to user emotions can significantly enhance engagement and effectiveness.

The field of education stands to benefit from these advancements as well. Emotion recognition systems could be used to gauge student engagement and comprehension in real-time, allowing educators to adjust their teaching methods dynamically. This could lead to more effective learning environments, where instructional strategies are continually optimized based on student emotional feedback.

In the realm of marketing and entertainment, emotion recognition technologies could provide deeper insights into consumer preferences and responses. Marketers could tailor their strategies based on emotional data, creating more compelling and targeted campaigns. Similarly, the entertainment industry could use emotion recognition to develop content that resonates more strongly with audiences, enhancing the overall viewer experience.

As researchers continue to push the boundaries of technology and methodology, the future of emotion recognition from EEG signals looks promising. Advanced signal processing techniques, such as continuous wavelet transform (CWT), and sophisticated machine learning models, including deep learning architectures, are likely to further enhance the accuracy and robustness of these systems. The integration of multimodal data, combining EEG with other physiological signals, will also provide a more comprehensive understanding of emotional states.

In conclusion, the ongoing advancements in EEG-based emotion recognition hold significant potential for transforming various domains. By enabling more accurate and real-time emotion monitoring, these technologies can improve mental health care, enhance human-computer interactions, and offer new insights and capabilities in education, marketing, and entertainment. The future of this field promises to deliver impactful and widespread benefits, shaping a more emotionally responsive and adaptive technological landscape.

# References

- [1] Zhang, Y., Zhang, S. and Ji, X., 2018. EEG-based classification of emotions using empirical mode decomposition and autoregressive model. *Multimedia Tools and Applications*, 77, pp.26697-26710
- [2] Li, Y., Huang, J., Zhou, H. and Zhong, N., 2017. Human emotion recognition with electroencephalographic multidimensional features by hybrid deep neural networks. *Applied Sciences*, 7(10), p.1060.
- [3] Islam, M.R., Moni, M.A., Islam, M.M., Rashed-Al-Mahfuz, M., Islam, M.S., Hasan, M.K., Hossain, M.S., Ahmad, M., Uddin, S., Azad, A. and Alyami, S.A., 2021. Emotion recognition from EEG signal focusing on deep learning and shallow learning techniques. *IEEE Access*, 9, pp.94601-94624.
- [4] Chen, J.X., Zhang, P.W., Mao, Z.J., Huang, Y.F., Jiang, D.M. and Zhang, Y.N., 2019. Accurate EEG-based emotion recognition on combined features using deep convolutional neural networks. *IEEE Access*, 7, pp.44317-44328.
- [5] Garg, D. and Verma, G.K., 2020. Emotion recognition in valence-arousal space from multi-channel EEG data and wavelet based deep learning framework. *Procedia Computer Science*, 171, pp.857-867.
- [6] Topic, A. and Russo, M., 2021. Emotion recognition based on EEG feature maps through deep learning network. *Engineering Science and Technology, an International Journal*, 24(6), pp.1442-1454.
- [7] Mert, A. and Akan, A., 2018. Emotion recognition from EEG signals by using multivariate empirical mode decomposition. *Pattern Analysis and Applications*, 21, pp.81-89.
- [8] Ali, M., Mosa, A.H., Al Machot, F. and Kyamakya, K., 2016, July. EEG-based emotion recognition approach for e-healthcare applications. In *2016 eighth international conference on ubiquitous and future networks (ICUFN)* (pp. 946-950). IEEE.
- [9] Hatamikia, S., Maghooli, K. and Nasrabadi, A.M., 2014. The emotion recognition system based on autoregressive model and sequential forward feature selection of electroencephalogram signals. *Journal of Medical Signals and Sensors*, 4(3), pp.194-201.
- [10] Huang, N.E., Shen, Z., Long, S.R., Wu, M.C., Shih, H.H., Zheng, Q., Yen, N.C., Tung, C.C. and Liu, H.H., 1998. The empirical mode decomposition and the Hilbert spectrum for nonlinear and non-stationary time series analysis. *Proceedings of the Royal Society of London. Series A: mathematical, physical and engineering sciences*, 454(1971), pp.903-995.

- [11] Jenke, R., Peer, A. and Buss, M., 2014. Feature extraction and selection for emotion recognition from EEG. *IEEE Transactions on Affective computing*, 5(3), pp.327-339.
- [12] Guo, K., Mei, H., Xie, X. and Xu, X., 2019, May. A convolutional neural network feature fusion framework with ensemble learning for EEG-based emotion classification. In *2019 IEEE MTT-S International Microwave Biomedical Conference (IMBioC)* (Vol. 1, pp. 1-4). IEEE.
- [13] Healey, J.A. and Picard, R.W., 2005. Detecting stress during real-world driving tasks using physiological sensors. *IEEE Transactions on intelligent transportation systems*, 6(2), pp.156-166.
- [14] Katsis, C.D., Katertsidis, N., Ganiatsas, G. and Fotiadis, D.I., 2008. Toward emotion recognition in car-racing drivers: A biosignal processing approach. *IEEE Transactions on Systems, Man, and Cybernetics-Part A: Systems and Humans*, 38(3), pp.502-512.
- [15] Murugappan, M., Ramachandran, N. and Sazali, Y., 2010. Classification of human emotion from EEG using discrete wavelet transform. *Journal of biomedical science and engineering*, 3(04), p.390.
- [16] Shukla, J., Barreda-Angeles, M., Oliver, J., Nandi, G.C. and Puig, D., 2019. Feature extraction and selection for emotion recognition from electrodermal activity. *IEEE Transactions on Affective Computing*, 12(4), pp.857-869.
- [17] Zhuang, N., Zeng, Y., Tong, L., Zhang, C., Zhang, H. and Yan, B., 2017. Emotion recognition from EEG signals using multidimensional information in EMD domain. *BioMed research international*, 2017.
- [18] Zangeneh Soroush, M., Maghooli, K., Kamaledin Setarehdan, S. and Nasrabadi, A.M., 2017. A review on EEG signals based emotion recognition. *International Clinical Neuroscience Journal*, 4(4), pp.118-129.
- [19] Degirmenci, M., Ozdemir, M.A., Sadighzadeh, R. and Akan, A., 2018, November. Emotion recognition from EEG signals by using empirical mode decomposition. In *2018 Medical Technologies National Congress (TIPTEKNO)* (pp. 1-4). IEEE.
- [20] Mikuckas, A., Mikuckiene, I., Venckauskas, A., Kazanavicius, E., Lukas, R. and Plauska, I., 2014. Emotion recognition in human computer interaction systems. *Elektronika ir Elektrotechnika*, 20(10), pp.51-56.
- [21] Chen, Y.F., Cui, Y.L. and Wang, S.X., 2017. Review of emotion recognition based on physiological signals. *System Simulation Technology*, 13(1), pp.1-5.
- [22] Li, J., Liu, G.Z. and Gao, J., 2017. Emotion classification based on EEG signal. *J. Beijing Univ. Inf. Sci. Technol.*, 32(2), pp.34-39.
- [23] Atkinson, J. and Campos, D., 2016. Improving BCI-based emotion recognition by combining EEG feature selection and kernel classifiers. *Expert Systems with Applications*, 47, pp.35-41.

- [24] Tripathi, S., Acharya, S., Sharma, R., Mittal, S. and Bhattacharya, S., 2017, February. Using deep and convolutional neural networks for accurate emotion classification on DEAP data. In Proceedings of the AAAI Conference on Artificial Intelligence (Vol. 31, No. 2, pp. 4746-4752).
- [25] Lan, Z., Sourina, O., Wang, L., Scherer, R. and Müller-Putz, G.R., 2018. Domain adaptation techniques for EEG-based emotion recognition: a comparative work on two public datasets. *IEEE Transactions on Cognitive and Developmental Systems*, 11(1), pp.85-94.
- [26] Qing, C., Qiao, R., Xu, X. and Cheng, Y., 2019. Interpretable emotion recognition using EEG signals. *Ieee Access*, 7, pp.94160-94170.
- [27] Hadjidimitriou, S.K. and Hadjileontiadis, L.J., 2012. Toward an EEG-based recognition of music liking using time-frequency analysis. *IEEE Transactions on Biomedical Engineering*, 59(12), pp.3498-3510.
- [28] Hjorth, B., 1970. EEG analysis based on time domain properties. *Electroencephalography and clinical neurophysiology*, 29(3), pp.306-310.